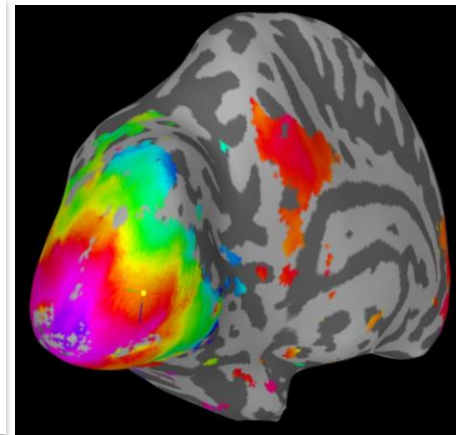
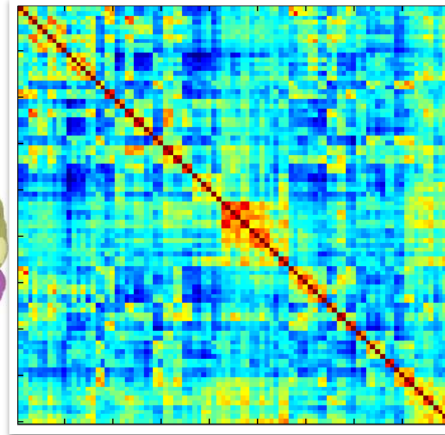
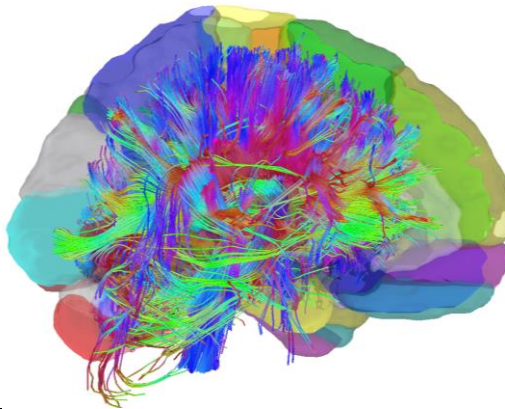
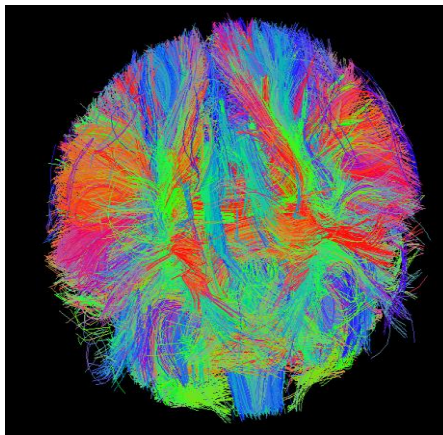


# *Exploring Human Brain Networks with Advanced MR Neuroimaging Technology*



***Li-Wei Kuo***

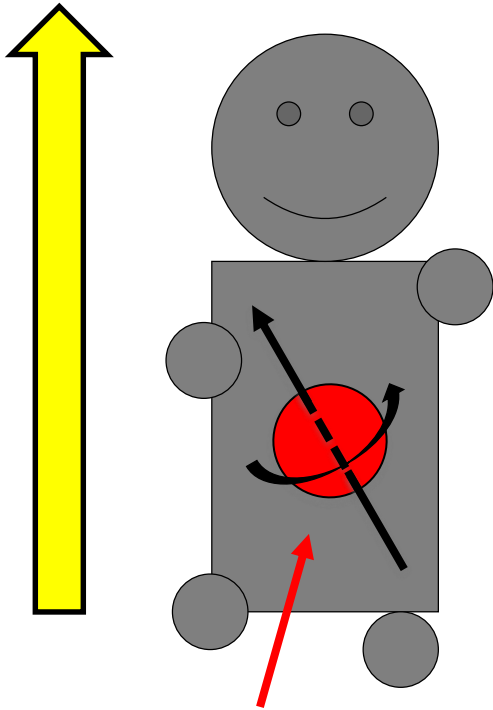
**Institute of Biomedical Engineering and Nanomedicine  
(I-BEN), National Health Research Institutes (NHRI)**

**2018/6/27 @BDHS**

# The theory of MRI

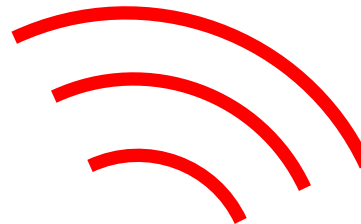
**M** = *Magnetic*    **R** = *Resonance*    **I** = *Imaging*

*Magnetic field direction*

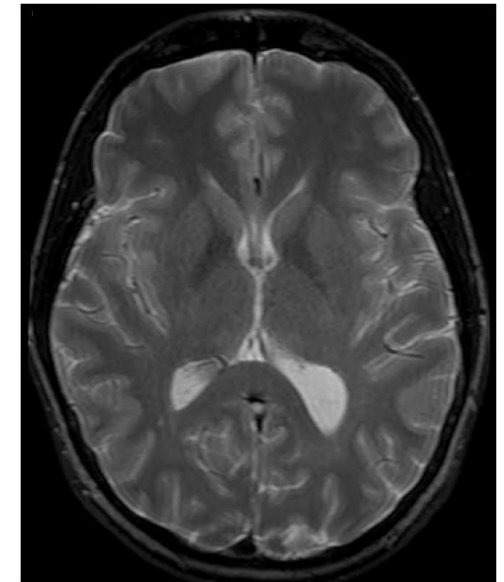


Proton: like a small magnet  
Water: 70% of human body

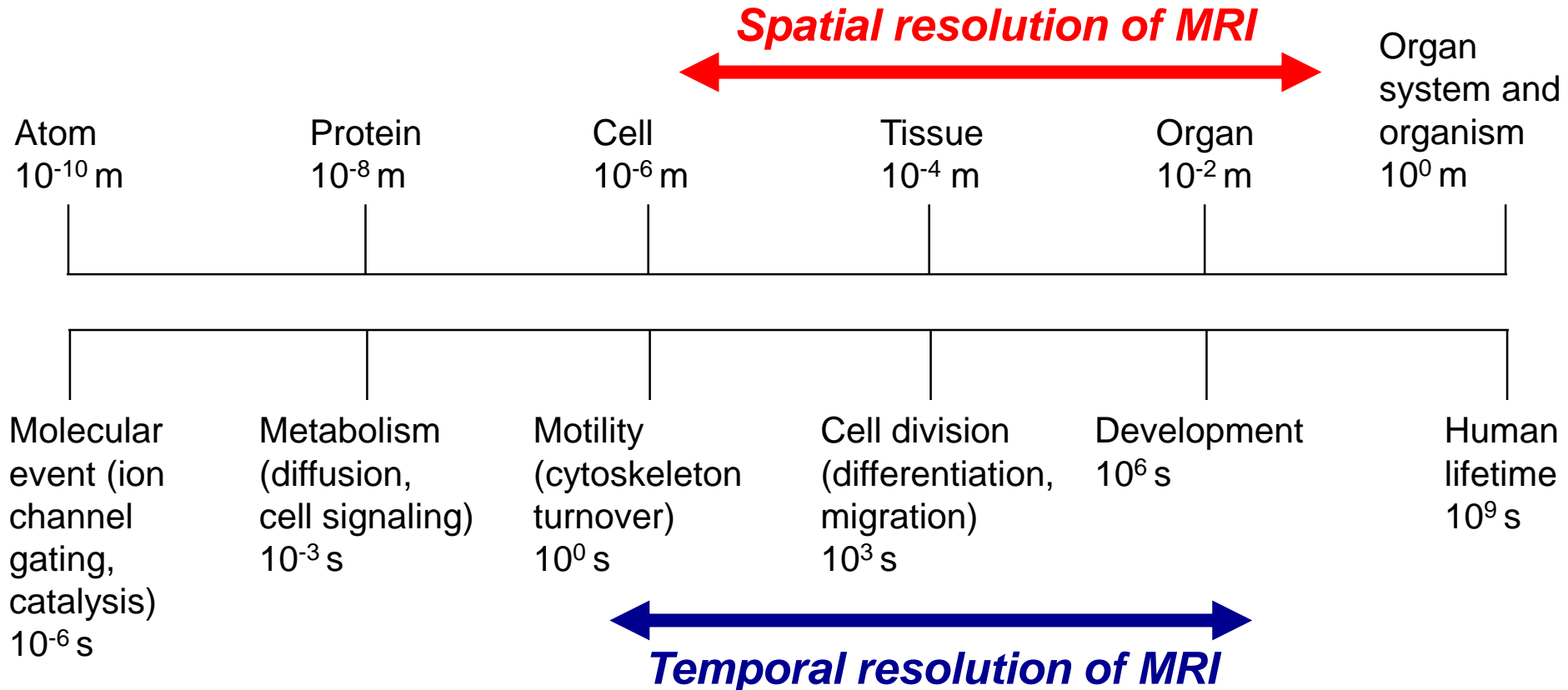
Same frequency



1.5T MRI: 63.5 MHz;  
3T MRI: 127 MHz



# Spatial and temporal scales in biological systems



- Sporns, "Discovering the Human Connectome," p6.

# Why MRI?

- Non-invasive (*safe and no harm*)
- Non-radioactive (*good for research*)
- Adequate spatial and temporal resolution for imaging biological tissues ( $\mu\text{m}\sim\text{mm}$ ,  $\text{ms}\sim\text{s}$ )
- Quantitative physical/physiological contrasts (*spin density, relaxation time, susceptibility, perfusion, diffusion, flow velocity, temperature, etc ...*)
- From animal to human (*good for translational research*)

# How the advanced computational technology changes MRI?

- *With the advancement of computational power and methodology, the development of MRI technology has been revolutionized during the past few year*



- Faster scan
- Higher throughput
- Multi-parametric contrast manipulation

- Undersampled data recon.
- Denoising
- Resolution enhancement
- Segmentation

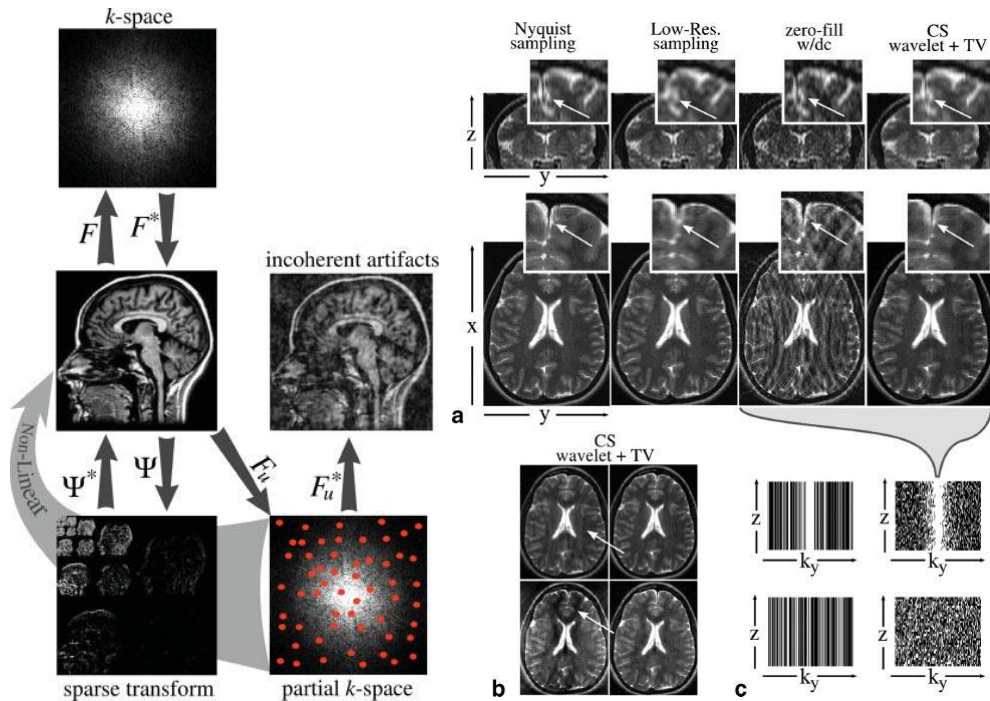
- Multi-modal parametric training and model establishment
- Classification
- Prediction

# Data Acquisition

Magnetic Resonance in Medicine 58:1182–1195 (2007)

## Sparse MRI: The Application of Compressed Sensing for Rapid MR Imaging

Michael Lustig,<sup>1\*</sup> David Donoho,<sup>2</sup> and John M. Pauly<sup>1</sup>



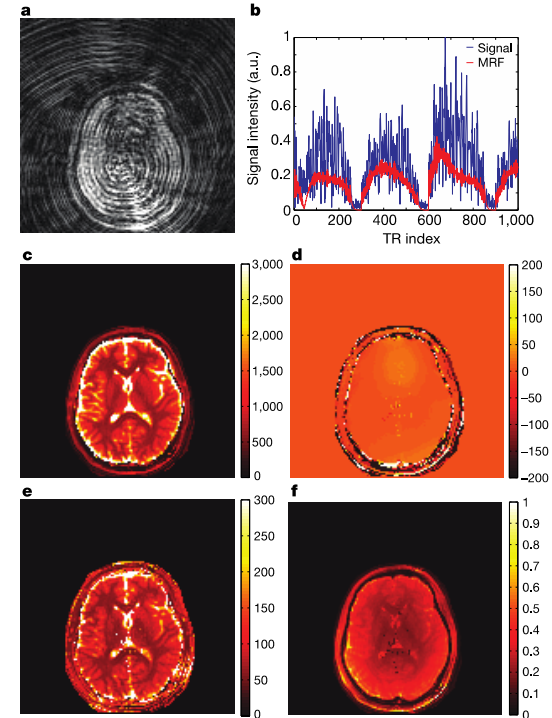
- Lustig et al., Mag Reson Med 2007

## ARTICLE

doi:10.1038/nature11971

## Magnetic resonance fingerprinting

Dan Ma<sup>1</sup>, Vikas Gulani<sup>1,2</sup>, Nicole Seiberlich<sup>1</sup>, Kecheng Liu<sup>3</sup>, Jeffrey L. Sunshine<sup>2</sup>, Jeffrey L. Duerk<sup>1,2</sup> & Mark A. Griswold<sup>1,2</sup>



- Ma et al., Nature 2013

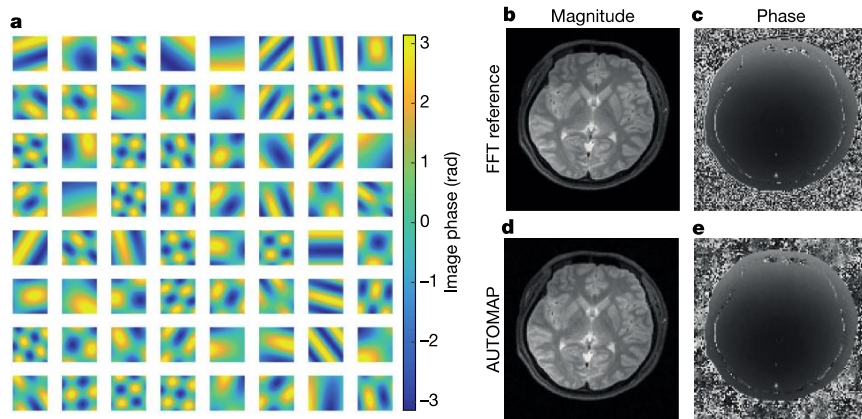
# Image Processing

LETTER

doi:10.1038/nature25988

## Image reconstruction by domain-transform manifold learning

Bo Zhu<sup>1,2,3</sup>, Jeremiah Z. Liu<sup>4</sup>, Stephen F. Cauley<sup>1,2</sup>, Bruce R. Rosen<sup>1,2</sup> & Matthew S. Rosen<sup>1,2,3</sup>



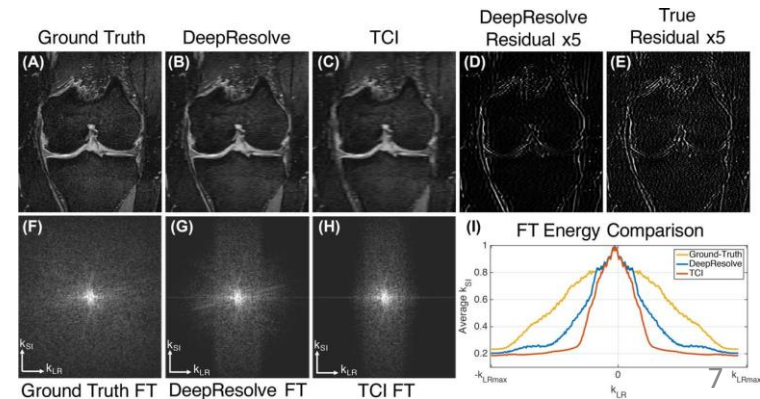
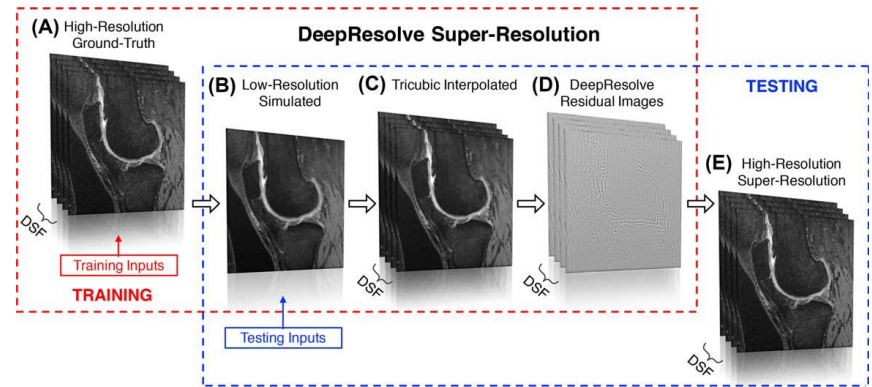
Received: 16 December 2017 | Revised: 14 February 2018 | Accepted: 22 February 2018  
DOI: 10.1002/mrm.27178

FULL PAPER

Magnetic Resonance in Medicine

## Super-resolution musculoskeletal MRI using deep learning

Akshay S. Chaudhari<sup>1,2,\*</sup> | Zhongnan Fang<sup>3,\*</sup> | Feliks Kogan<sup>1</sup> | Jeff Wood<sup>1</sup> | Kathryn J. Stevens<sup>1,4</sup> | Eric K. Gibbons<sup>5</sup> | Jin Hyung Lee<sup>2,3,6,7</sup> | Garry E. Gold<sup>1,2,4</sup> | Brian A. Hargreaves<sup>1,2,7</sup>



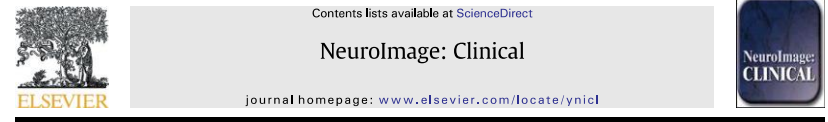
- Zhu et al., Nature 2018
- Chaudhari et al., Mag Reson Med 2017

# Data Analysis

NeuroImage 101 (2014) 569–582



NeuroImage: Clinical 13 (2017) 361–369

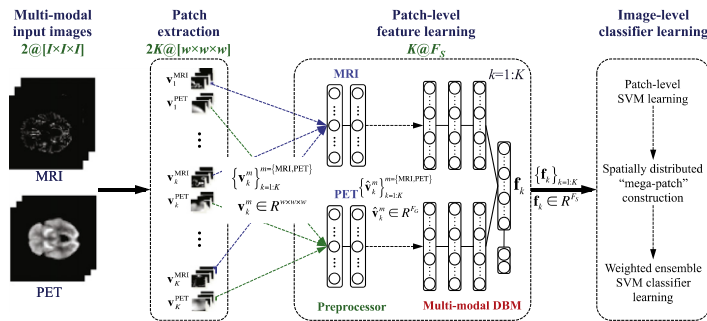


## Hierarchical feature representation and multimodal fusion with deep learning for AD/MCI diagnosis



Heung-Il Suk<sup>a</sup>, Seong-Whan Lee<sup>b</sup>, Dinggang Shen<sup>a,b,\*</sup>, the Alzheimer's Disease Neuroimaging Initiative<sup>1</sup>

<sup>a</sup> Department of Radiology and Biomedical Research Imaging Center (BRIC), University of North Carolina at Chapel Hill, NC, USA  
<sup>b</sup> Department of Brain and Cognitive Engineering, Korea University, Seoul, Republic of Korea



**Table 2**  
A summary of the performances of two methods. The boldface denotes the best performance in each metric for each classification task.

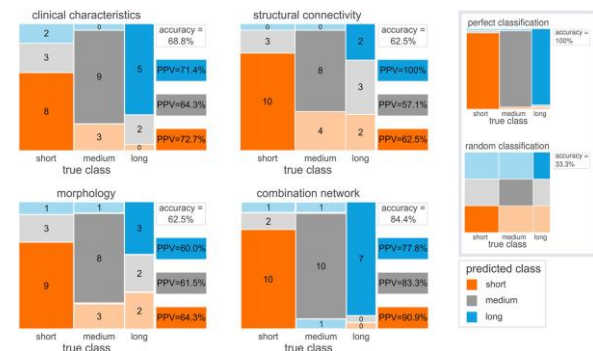
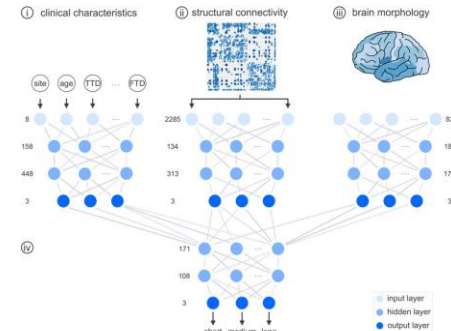
	Method	Modality	ACC (%)	SEN (%)	SPEC (%)	BAC (%)	PPV (%)	NPV (%)	AUC (%)
AD/NC	Liu et al.	MRI	90.18 ± 5.25	91.54	90.61	91.08	88.94	90.67	0.9620
		PET	89.13 ± 6.81	90.06	89.36	89.71	88.49	89.26	0.9594
	Proposed	MRI + PET	90.27 ± 7.02	89.48	92.44	90.96	90.56	88.70	0.9655
		MRI	92.38 ± 5.32	91.54	94.56	93.05	92.65	90.84	0.9697
		PET	92.20 ± 6.70	88.04	<b>96.33</b>	92.19	95.03	89.66	0.9798
		MRI + PET	<b>95.35 ± 5.23</b>	<b>94.65</b>	95.22	<b>94.93</b>	<b>96.80</b>	<b>95.67</b>	<b>0.9877</b>
MCI/NC	Liu et al.	MRI	81.00 ± 4.98	97.08	48.18	72.63	79.14	88.99	0.8352
		PET	81.14 ± 10.22	96.03	52.59	74.31	80.26	84.16	0.8231
	Proposed	MRI + PET	83.90 ± 5.80	98.97	52.59	75.78	81.18	97.22	0.8301
		MRI	84.24 ± 6.26	<b>99.58</b>	53.79	76.69	81.23	<b>98.75</b>	0.8478
		PET	84.29 ± 7.22	98.69	56.87	77.78	81.99	94.57	0.8297
		MRI + PET	<b>85.67 ± 5.22</b>	95.37	<b>65.87</b>	<b>80.62</b>	<b>85.02</b>	89.00	<b>0.8808</b>
MCI-C/MCI-NC	Liu et al.	MRI	64.75 ± 14.83	22.22	89.57	55.90	46.29	77.39	0.6355
		PET	67.17 ± 13.43	40.02	82.61	61.32	64.13	70.31	0.6911
	Proposed	MRI + PET	73.33 ± 12.47	33.25	<b>97.52</b>	65.38	80.00	73.18	0.7159
		MRI	72.42 ± 13.09	36.70	90.98	63.84	65.49	<b>77.84</b>	0.7342
		PET	70.75 ± 13.23	25.45	96.55	61.00	75.00	70.69	0.7215
		MRI + PET	<b>75.92 ± 15.37</b>	<b>48.04</b>	95.23	<b>71.63</b>	<b>83.50</b>	74.33	<b>0.7466</b>

## Deep learning predictions of survival based on MRI in amyotrophic lateral sclerosis



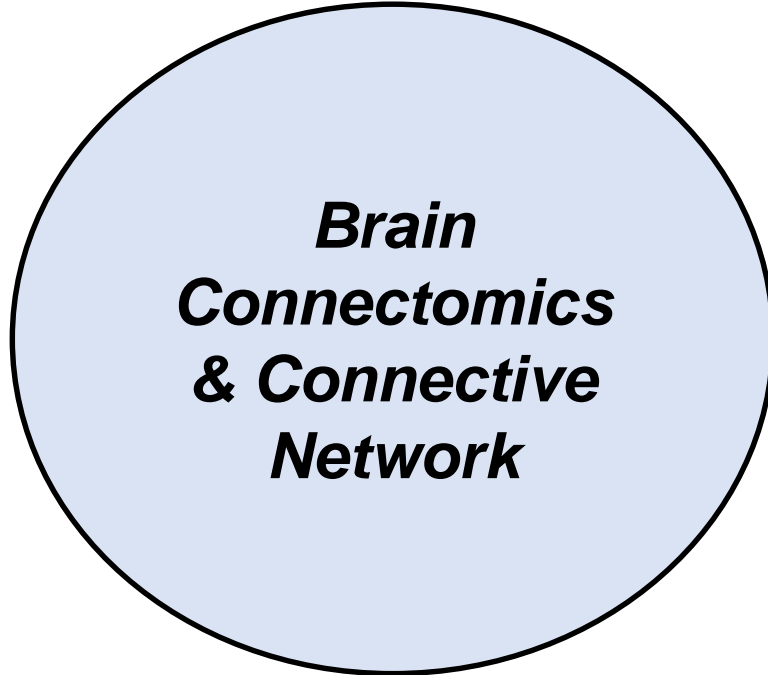
Hannelore K. van der Burgh<sup>1</sup>, Ruben Schmidt<sup>1</sup>, Henk-Jan Westeneng<sup>2</sup>, Marcel A. de Reus<sup>1</sup>, Leonard H. van den Berg<sup>1,2</sup>, Martijn P. van den Heuvel<sup>1,2</sup>

<sup>1</sup>Department of Neurology, Brain Center Rudolf Magnus, University Medical Center Utrecht, Heidelberglaan 100, PO Box 85500, 3508 GA, Utrecht, Netherlands  
<sup>2</sup>Department of Psychiatry, Brain Center Rudolf Magnus, University Medical Center Utrecht, Heidelberglaan 100, PO Box 85500, 3508 GA, Utrecht, Netherlands

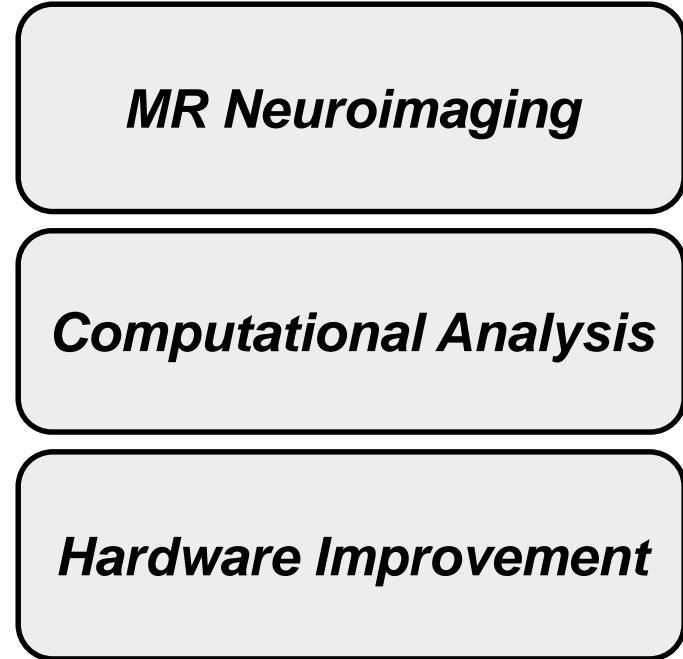




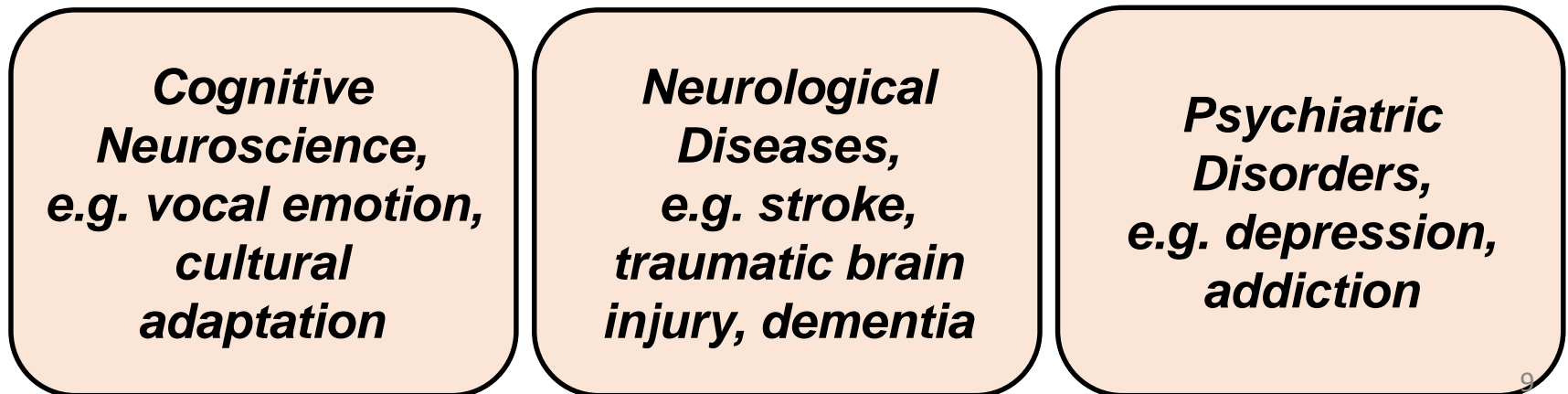
## Target



## Approaches



## Applications



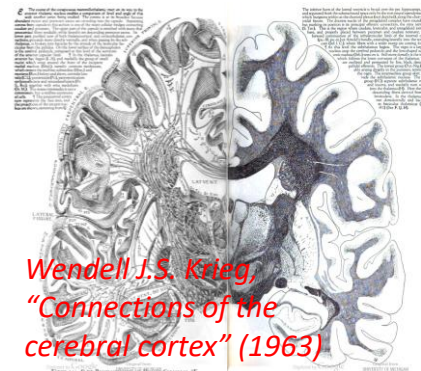
# Why Brain Research?

## A Challenging Target in 21<sup>st</sup> Century

The collage features several key elements related to brain research initiatives:

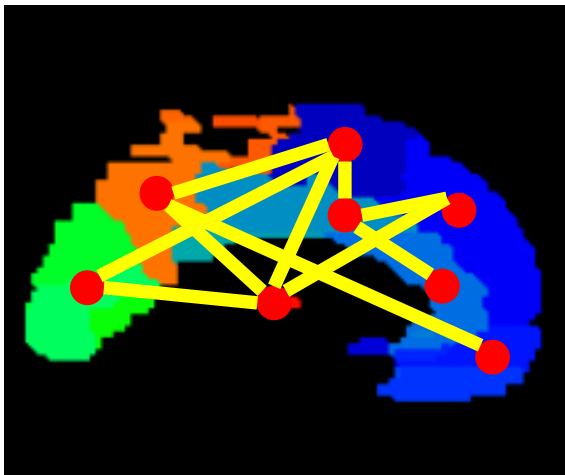
- NIH Brain Initiative:** A screenshot of the NIH website highlighting the "Brain Research through Advancing Innovative Neurotechnologies (BRAIN) Initiative". It includes text about the need for research and a colorful brain scan image.
- NIH Blueprint:** A logo for the "NIH Blueprint for Neuroscience Research".
- Human Connectome Project:** A central diagram with four interconnected circles labeled "Project", "Community", "Participate", and "Programme".
- CONNECT:** A screenshot of the "CONNECT - Consortium Of Neuroimagers for the Non-invasive Exploration of Brain Connectivity and Tracts" website, detailing its goals and the consortium's work.
- Harvard/MGH-UCLA Project:** A screenshot of the "The Harvard/MGH-UCLA Project" website, showing a colorful brain scan.
- Human Connectome Project Text:** A block of text explaining the project's purpose: "The NIH Human Connectome Project is an ambitious effort to map the neural pathways that underlie human brain function. The overarching purpose of the Project is to acquire and share data about the structural and functional connectivity of the human brain..."

- The research of “brain and mind” can help us understand how brain works and improve the diagnosis or treatment for brain diseases
- Non-invasive neuroimaging technologies can provide accurate and reproducible measurements of brain structures and functions



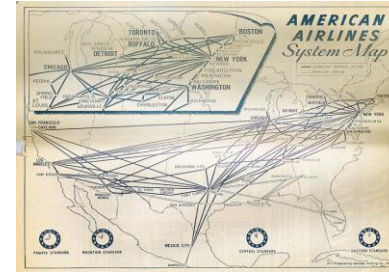
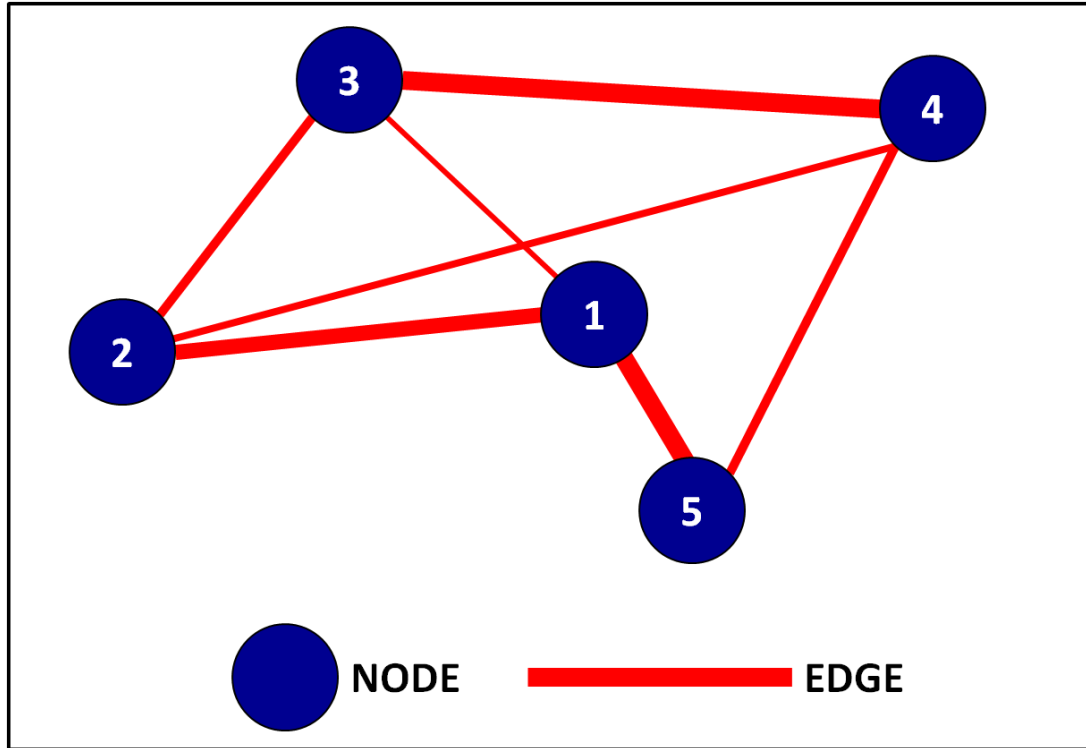
# “Connectome” at Multiple Scales

- **Brain connectome can be defined at different levels of scales, i.e. spatial resolution**
  - *Microscale: cellular level (neurons and synapses)*
  - *Mesoscale: circuits and cell populations*
  - *Macroscale: anatomical regions and pathways*
- ***Structural connectome* and *functional connectome***  
(Sporns et al., 2005; Biswal et al., 2010; Bullmore and Sporns, 2009)

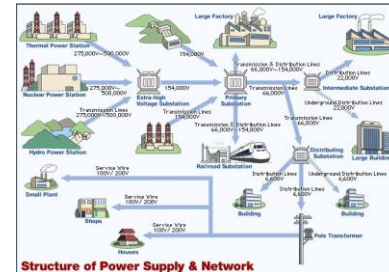


<i>Measurement</i>	<i>Edge representation</i>	<i>Empirical techniques</i>
<i>Structural connectivity</i>	<i>Presence/absence of physical links</i>	<i>Tract tracing, diffusion MRI, anatomical MRI</i>
<i>Functional connectivity</i>	<i>Statistical relationships between neural time courses</i>	<i>Neurophysiological recordings, EEG/MEG, BOLD fMRI</i>

# What is a “Network”?



Airway



Electricity

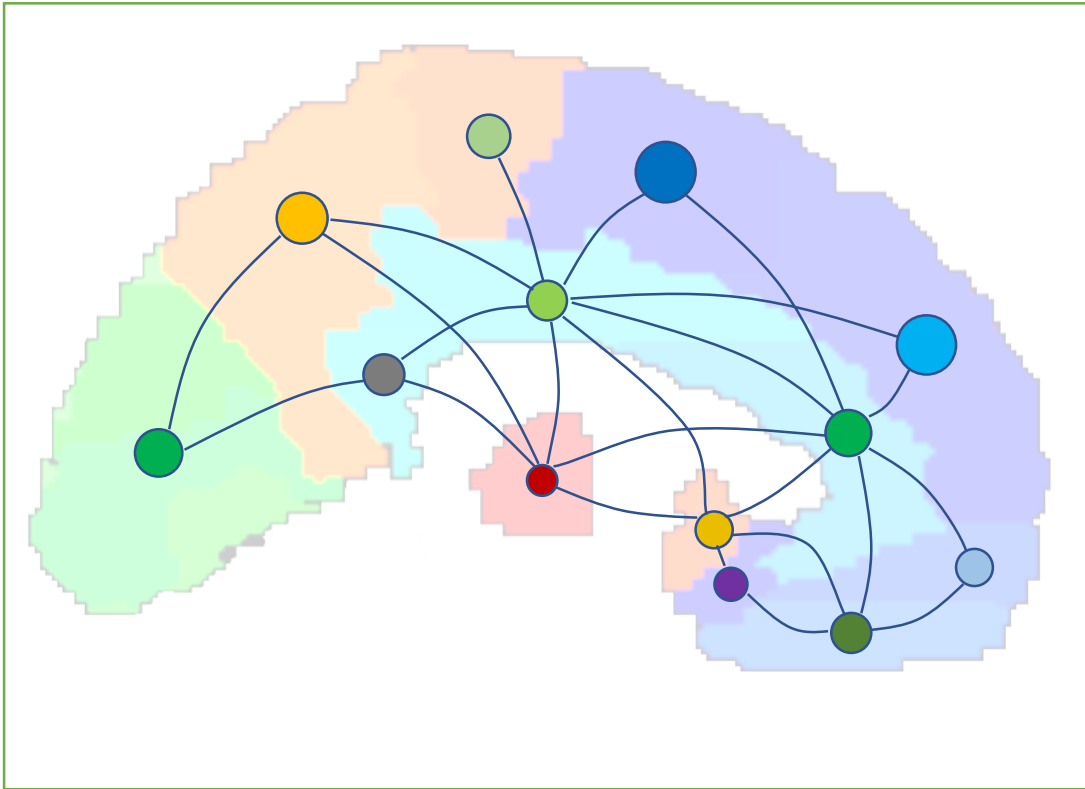


Social

Two important issues:

- How these nodes connect (structural connectivity)
- What happens between nodes (functional connectivity)

# ***Node and Edge for representing a Brain Network***



**Node –**

*Anatomical regions*

**Edge –**

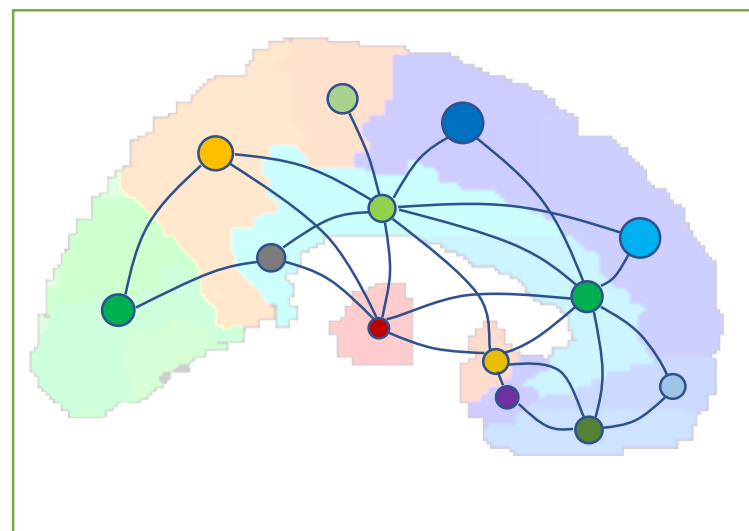
*Structural connectivity*  
*Functional connectivity*

*The basic concept is to compute nodes/edges from MRI data and measure the network characteristics of brain*

*How do we define the  
nodes of a brain network?*

# To define the “Nodes”

- *Network “**nodes**” can be represented by a group of cortical parcellations*
- *These cortical parcellations can be obtained by the following constraints*
  - ***Anatomical regions***
  - ***Structural connections***
  - ***Functional connectivity***

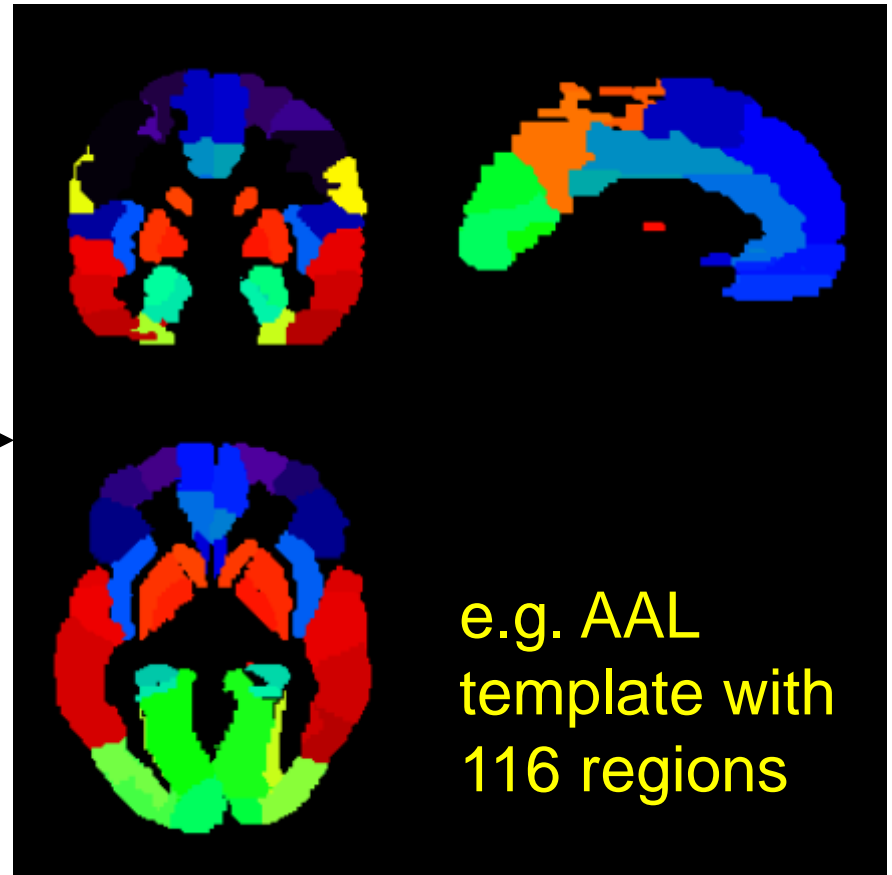


# We can easily get the “Nodes” from a brain anatomical atlas



Subject's 3DT1  
anatomical  
images

Registration  
to template



e.g. AAL  
template with  
116 regions



***How do we measure the structural connectivity?***

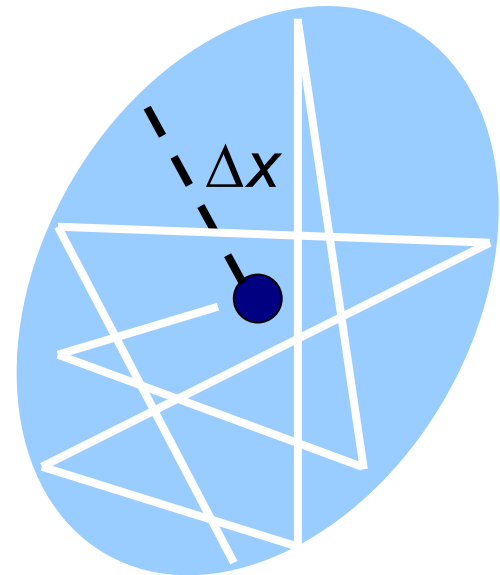
# Diffusion phenomena

***Microscopic random motion, i.e. Brownian motion***

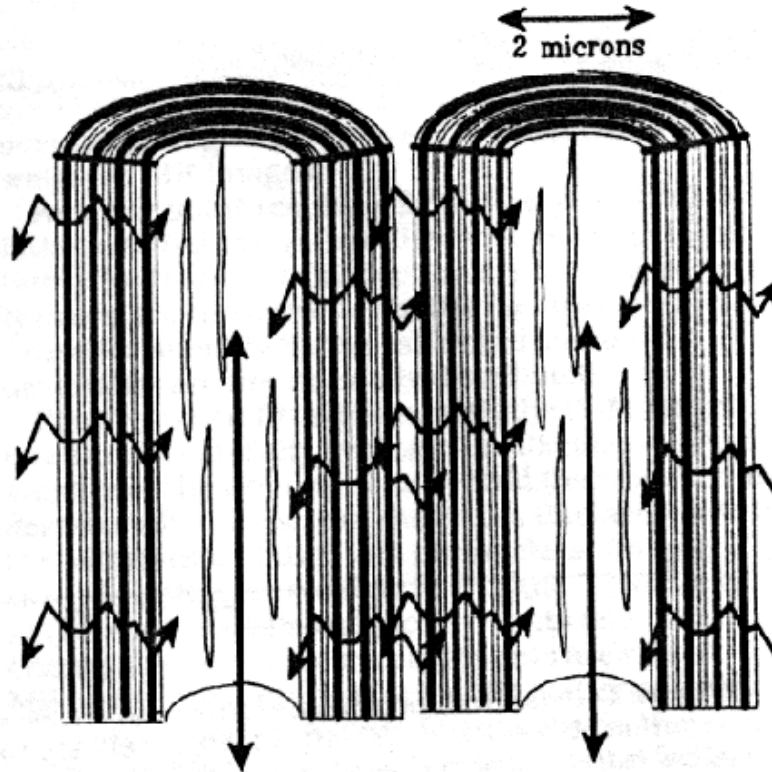
**To measure diffusion using MRI**

- **Pulsed gradient spin echo (PGSE)**
  - *Stejskal and Tanner, 1965*
- **Diffusion-weighted imaging (DWI)**
  - *Wesbey et al., 1984*
- **Diffusion tensor imaging (DTI)**
  - *Basser et al., 1994*
- **Diffusion spectrum imaging (DSI)**
  - *Wedeen et al., 2000*

$$\Delta x = \sqrt{2D\Delta t}$$

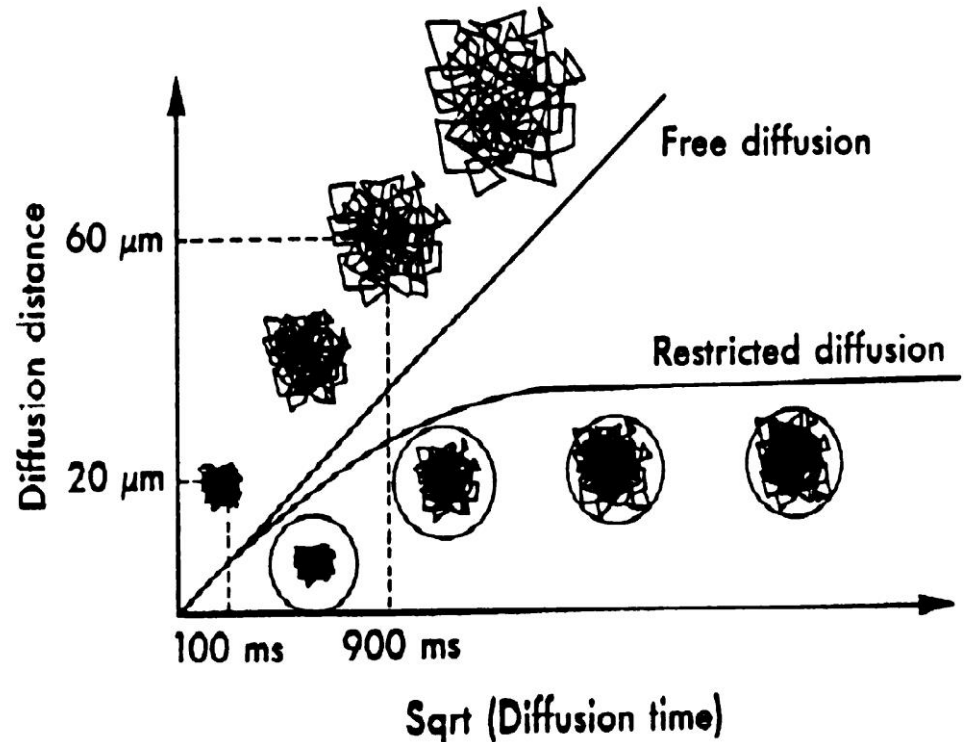


# Diffusion anisotropy in biological tissue, e.g. neural fibers



$$D_{||} = 1.2 \times 10^{-3} \text{ mm}^2/\text{s}$$

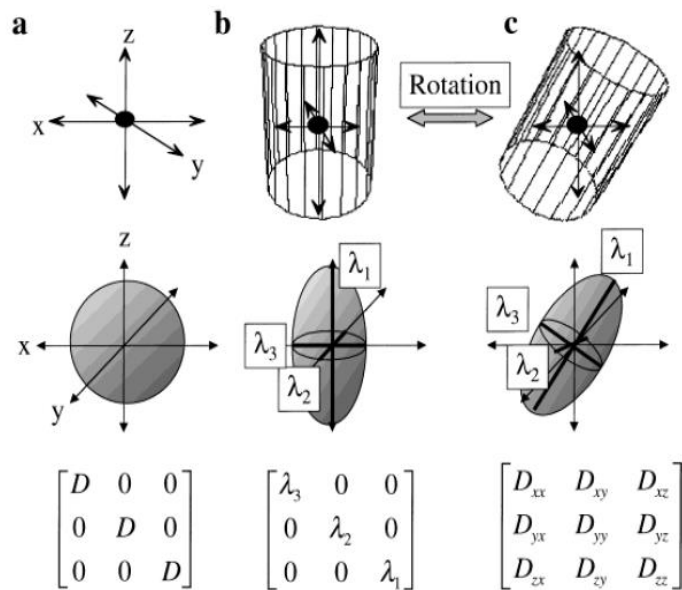
$$D_{\perp} = 0.4 \times 10^{-3} \text{ mm}^2/\text{s}$$



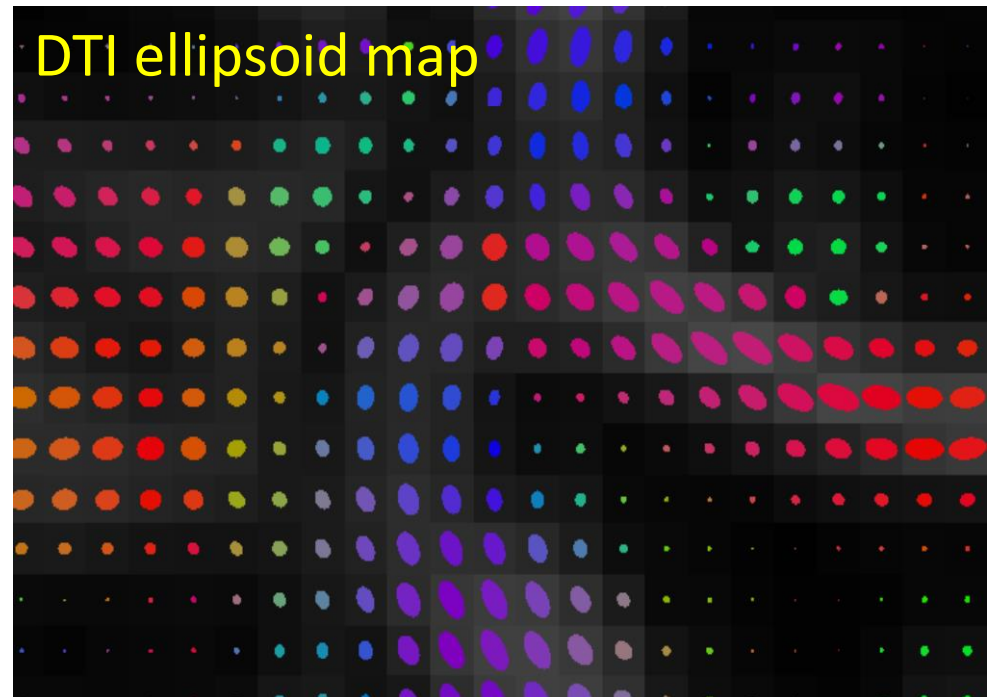
- Douek *et al.*, JCAT 1991

# Diffusion Tensor MRI (DTI)

- A widely used diffusion MRI approach to map the fiber orientations and white matter integrity (*Basser et al., Biophys J 1994*)



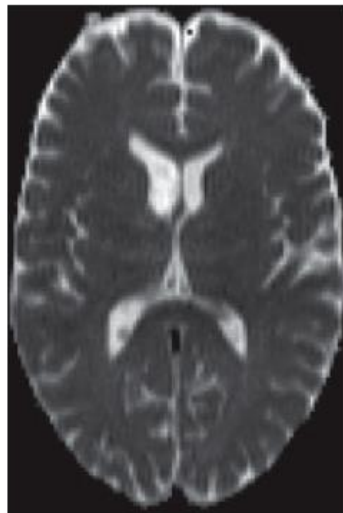
**DTI models the intravoxel fibers as a diffusion ellipsoid**



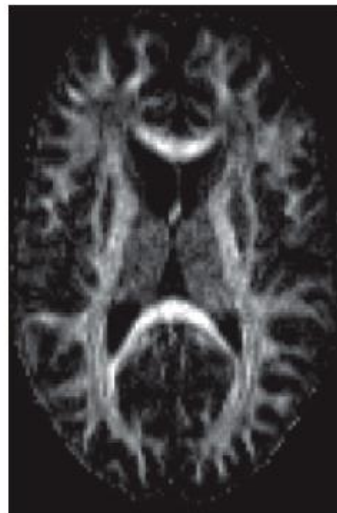
# DTI quantitative indices

- *These measures can represent the white matter integrity*

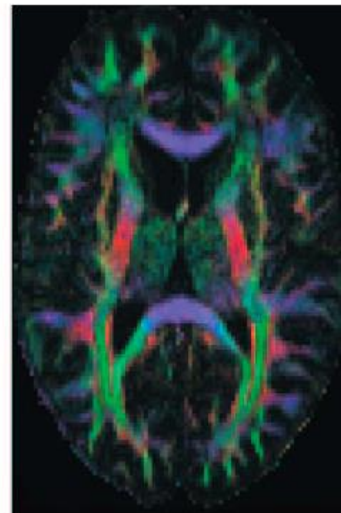
trADC



FA

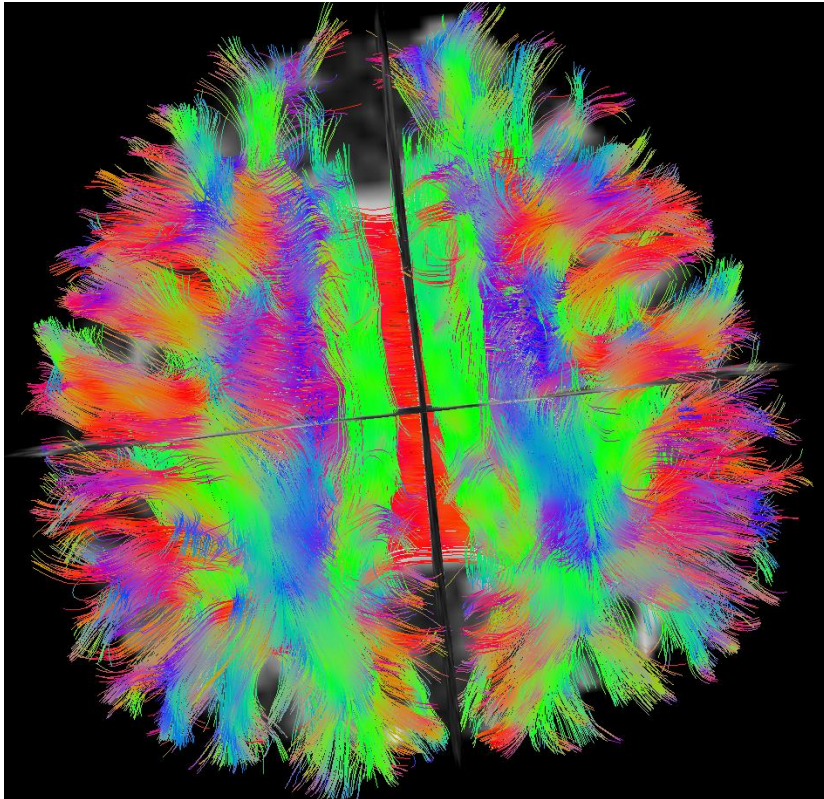


Colormap of  
1<sup>st</sup> eigenvector

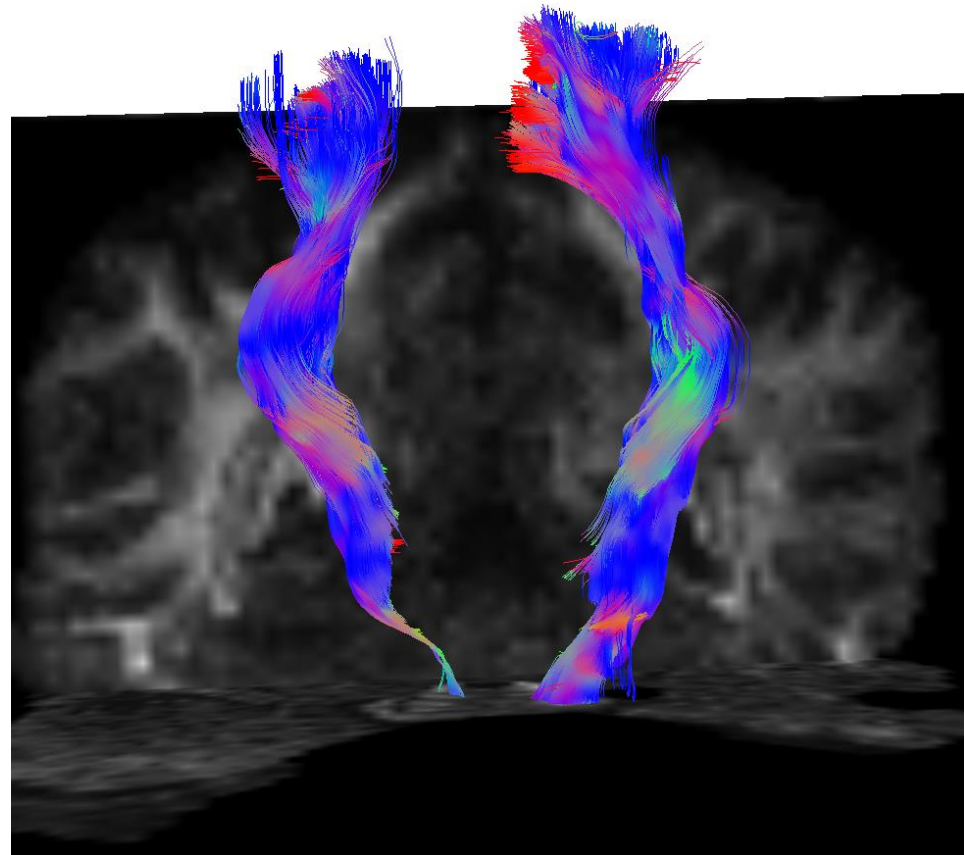


- Hagmann *et al.*, *RadioGraphics* 2006

# Diffusion MRI Fiber Tracking



**Whole Brain Tracts**

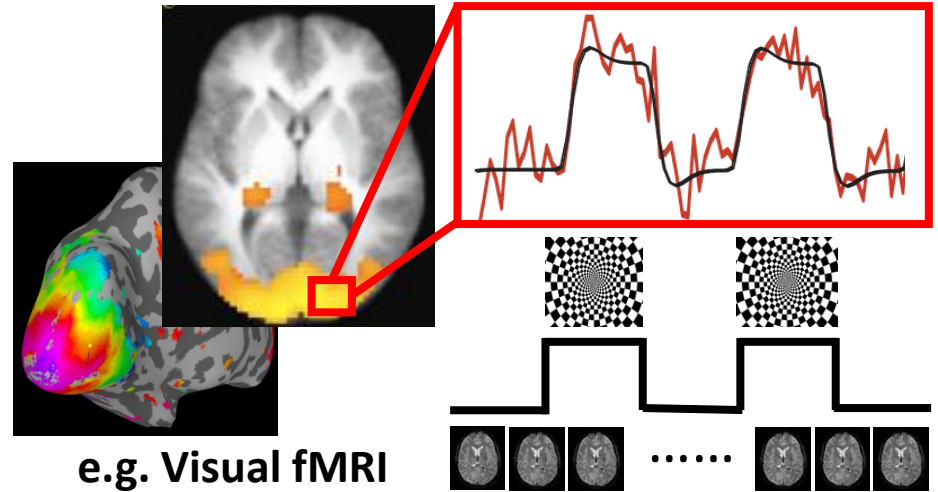
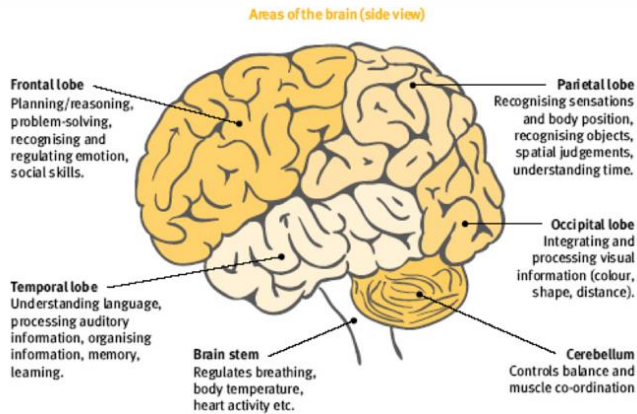


**Corticospinal Tract**

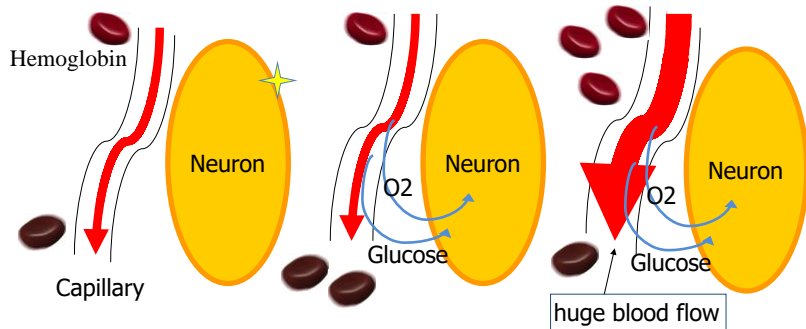
***How do we measure the functional connectivity?***

# BOLD Functional MRI

## Task-based fMRI

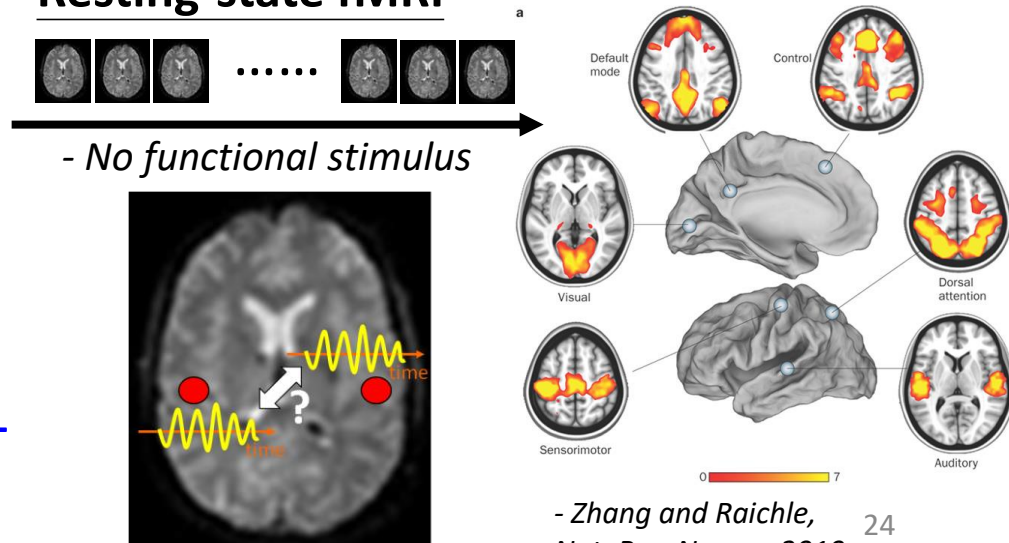


1. Neuronal activation
2. Extracting "fuel"
3. Blood "flood"



- fMRI: functional MRI
- BOLD contrast: blood-oxygenation-level-dependent contrast

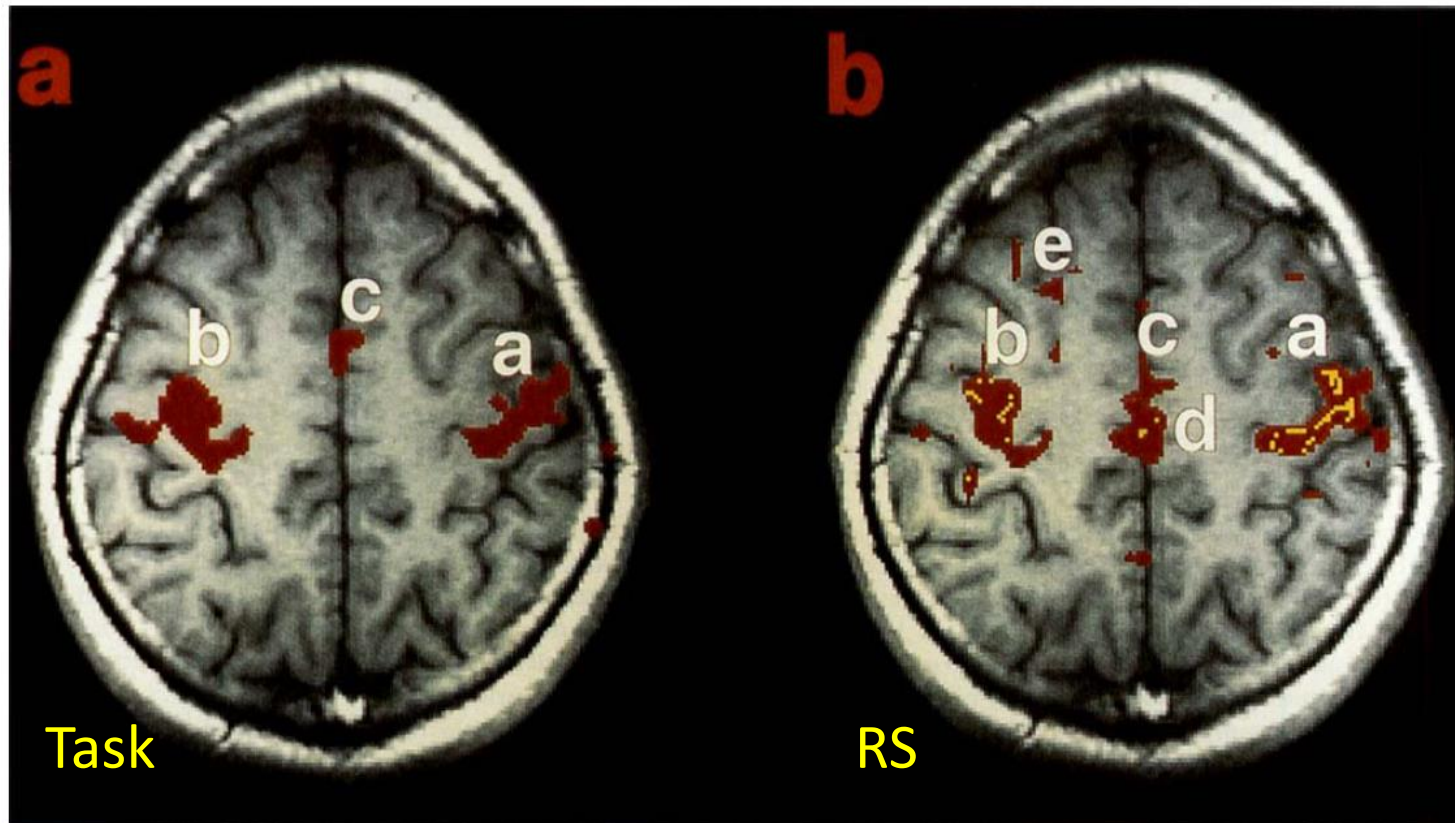
## Resting-state fMRI





# Resting-state fMRI: first evidence

RS-fMRI: not just noise

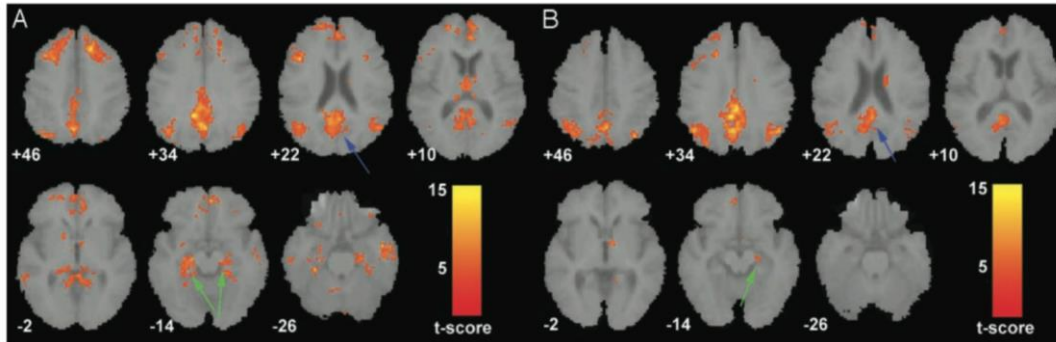


- Biswal et al., MRM 1995

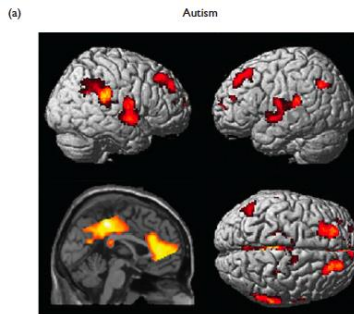
# Clinical applications with RS-fMRI

The resting human brain:

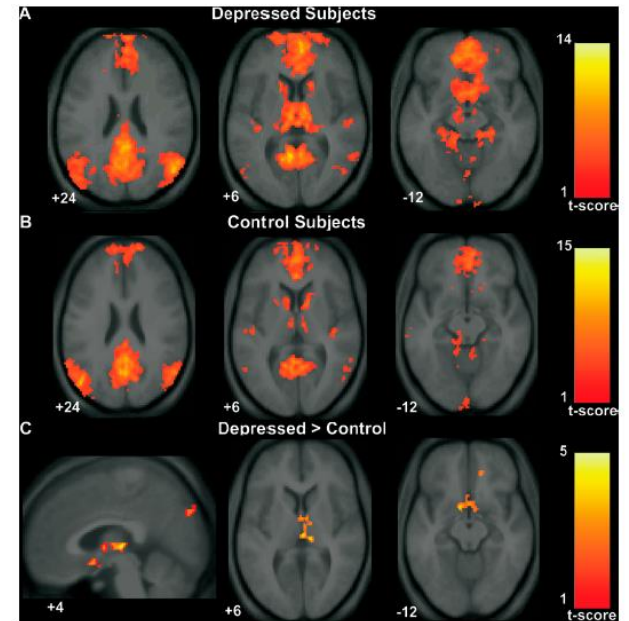
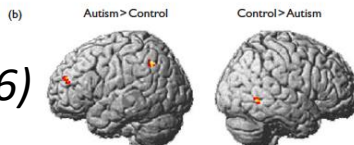
**represents 2% of total body mass but consumes 20% of the body's energy**



Healthy Elderly vs. Alzheimer's Disease (AD)  
(Greicius et al., PNAS 2004)



Healthy control vs. Autism  
(Cherkassky et al., NeuroReport 2006)



Healthy control vs. Depression  
(Greicius et al., Biol Psychiatry 2007)

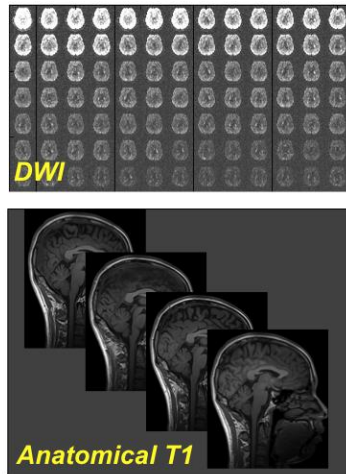
***Computational approaches.***

***Now we have nodes and  
edges.***

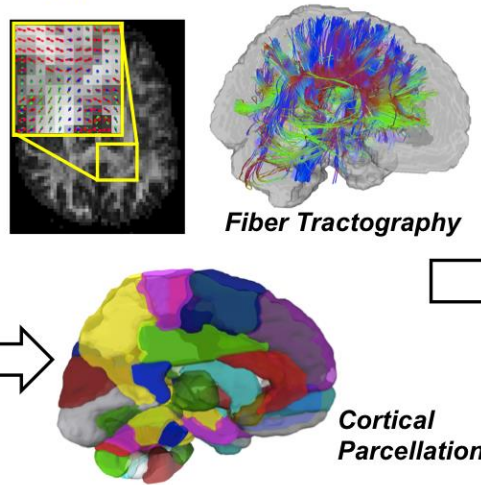
***How to analyze the brain  
network with graph theory?***

# Graph Theoretical Analysis of a Brain Network

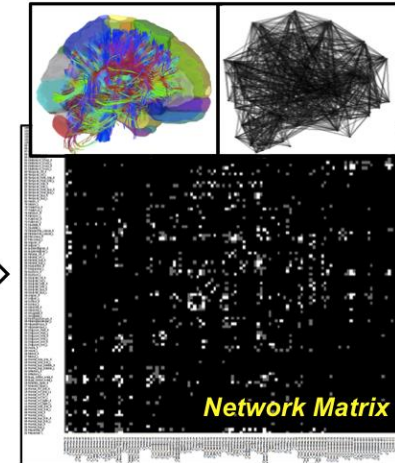
(a) MRI Data Acquisition



(b) Data Reconstruction



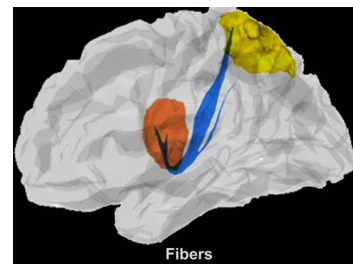
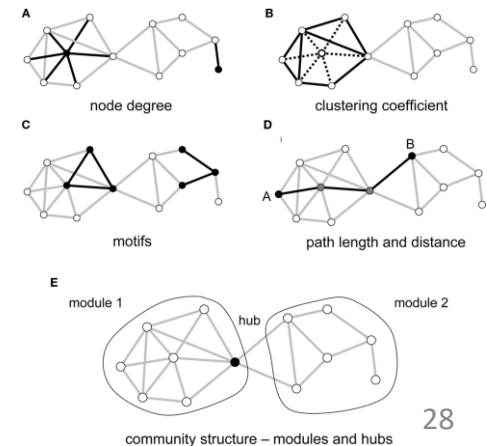
(c) Network Analysis



Define “Connectivity” between different cortical regions

- Fiber numbers
- Fiber density
- Fiber length
- Anisotropy
- Diffusivity

*Derive network properties with graph theory analysis*

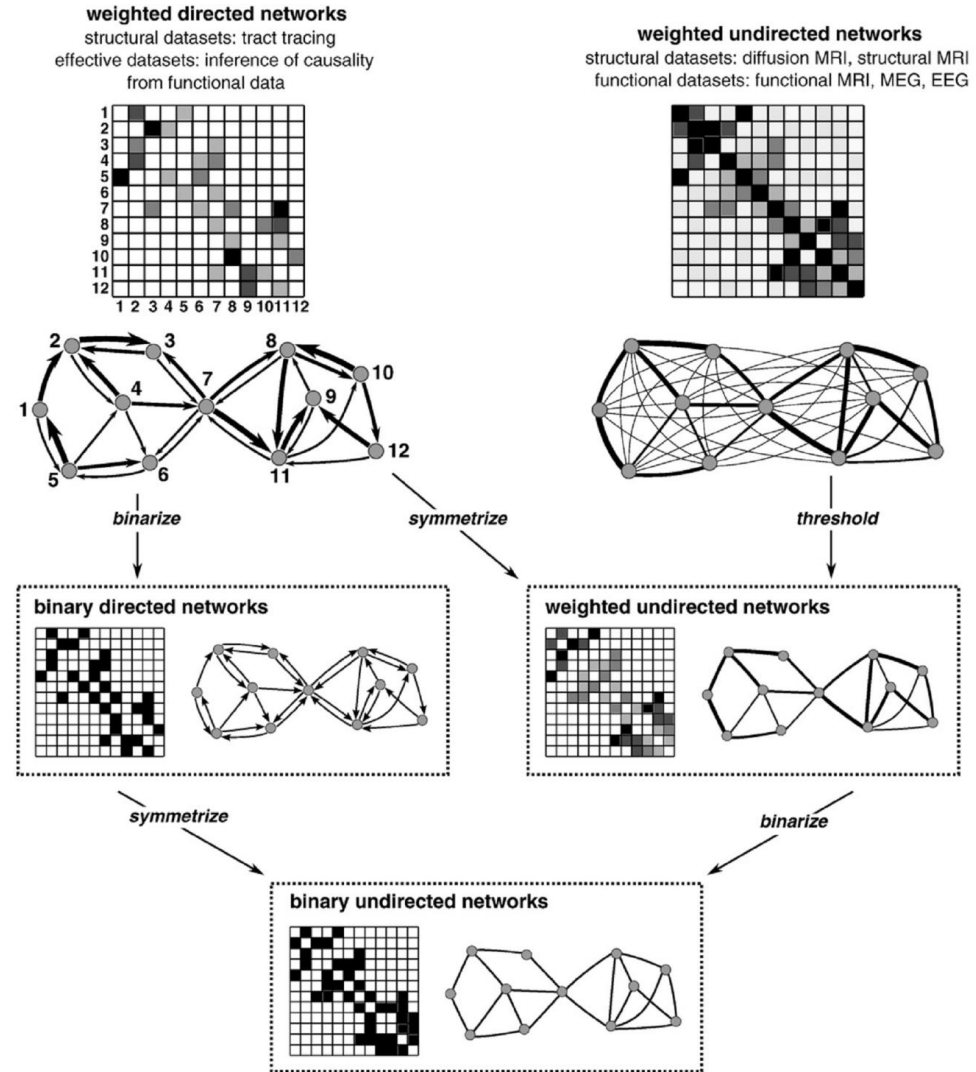


# Characteristics of a network

Weighted vs. Unweighted

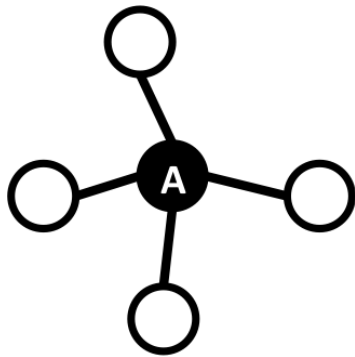
Directed vs. Undirected

Binarized

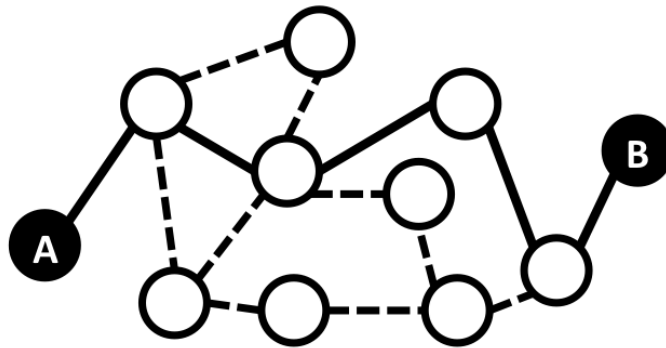


# Some simple network measures

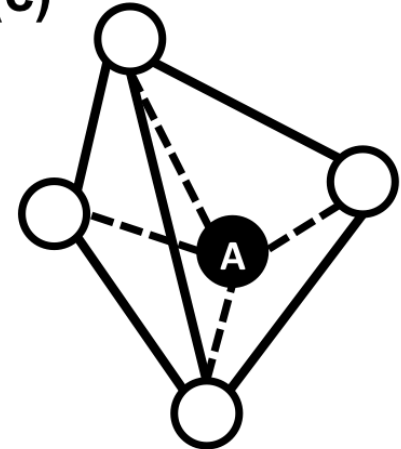
(a)



(b)



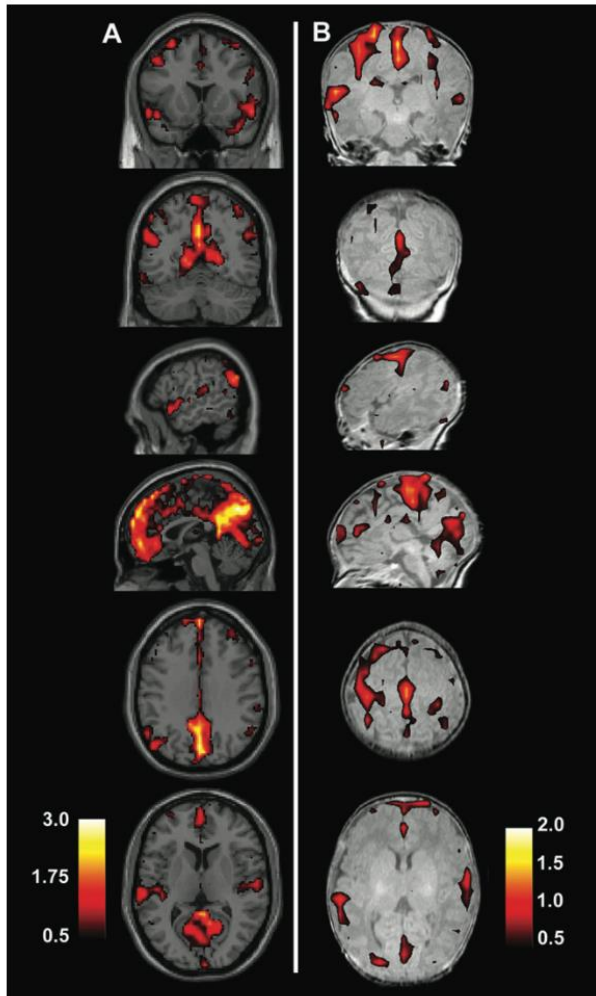
(c)



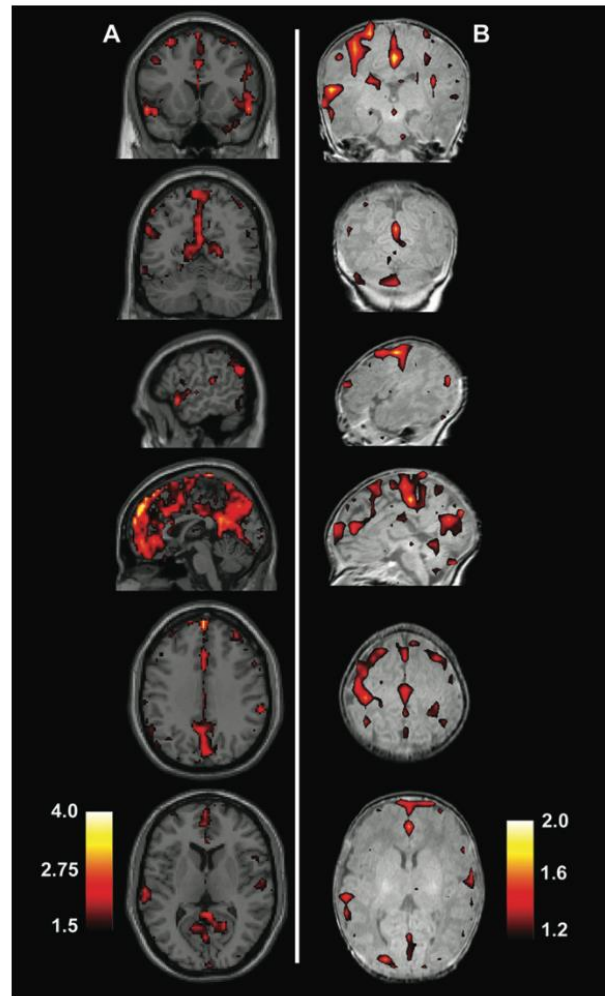
- (a) Degree: the degree of node A is 4
- (b) Shortest path length: the shortest path length between A and B is 5
- (c) Clustering coefficient: the clustering coefficient of node A is  $5/6$  ([# of connections / # of max connections] between all neighbor nodes)

# Brain Network in development

DEGREE Centrality



BETWEENNESS Centrality

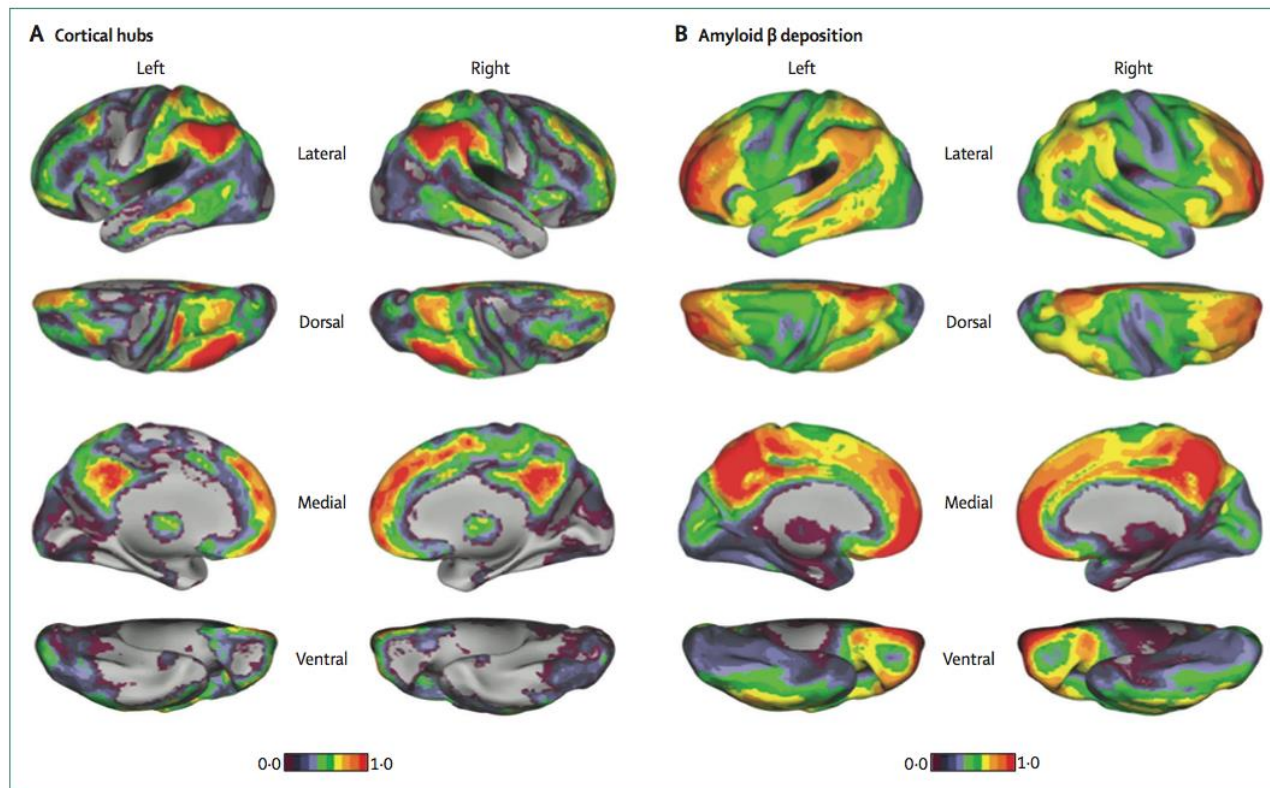


*To investigate infants' brain network using resting-state fMRI, the results show the centrality is higher in primary cortex regions to support early development*

*- Fransson et al.,  
Cerebral Cortex 2011*

# Network Centrality vs. A $\beta$ deposition

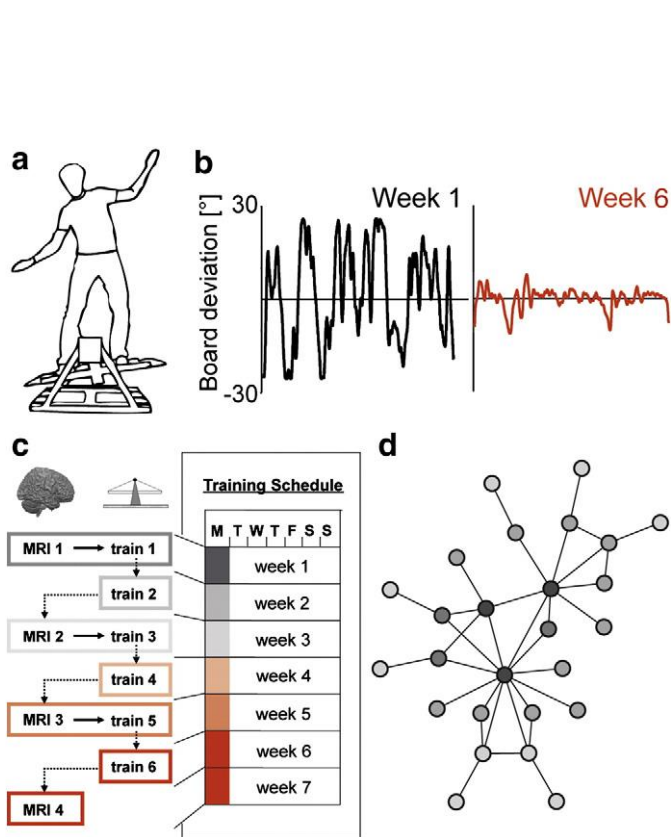
*The mappings of network centrality and A $\beta$  deposition show a similar pattern in several areas including posterior cingulate cortex, precuneus, inferior parietal lobe and medial frontal cortex*



- Buckner et al., J neurosci, 2009

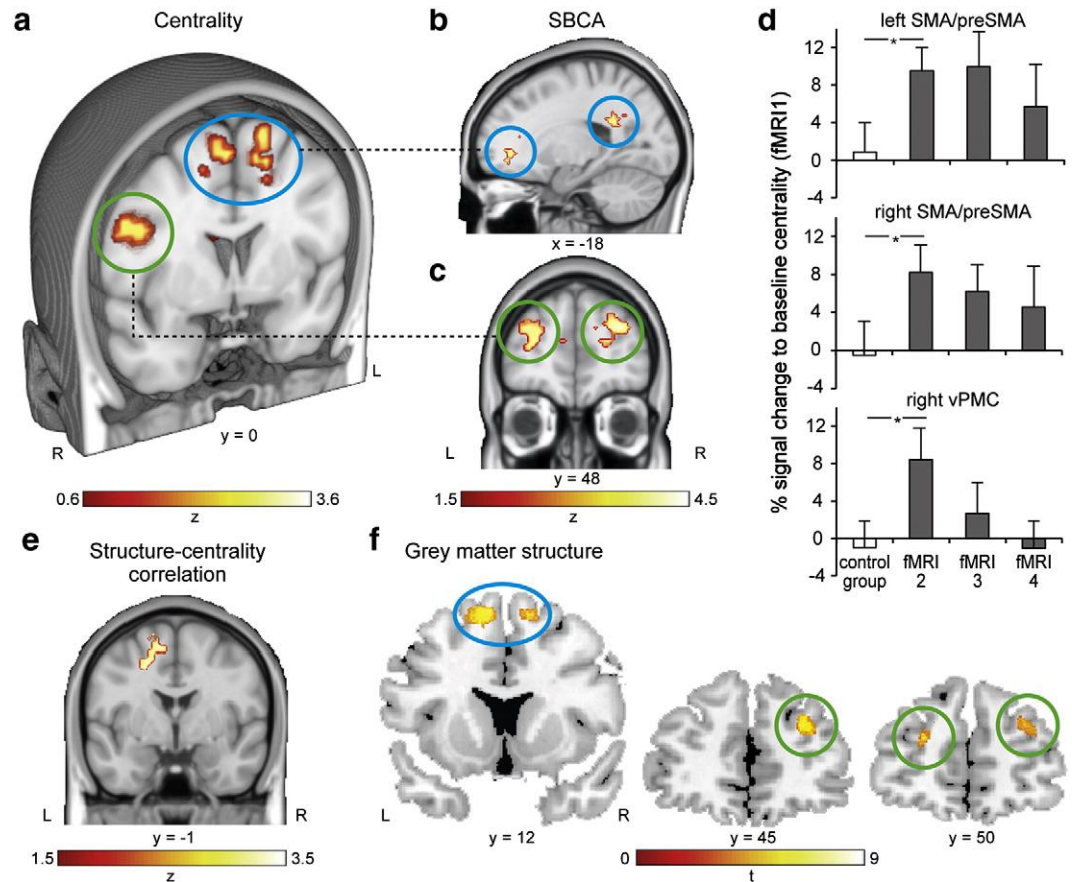


# Training vs. Brain Network



Training experiments

- Taubert et al., Neuroimage 2011



Increase of Network Centrality

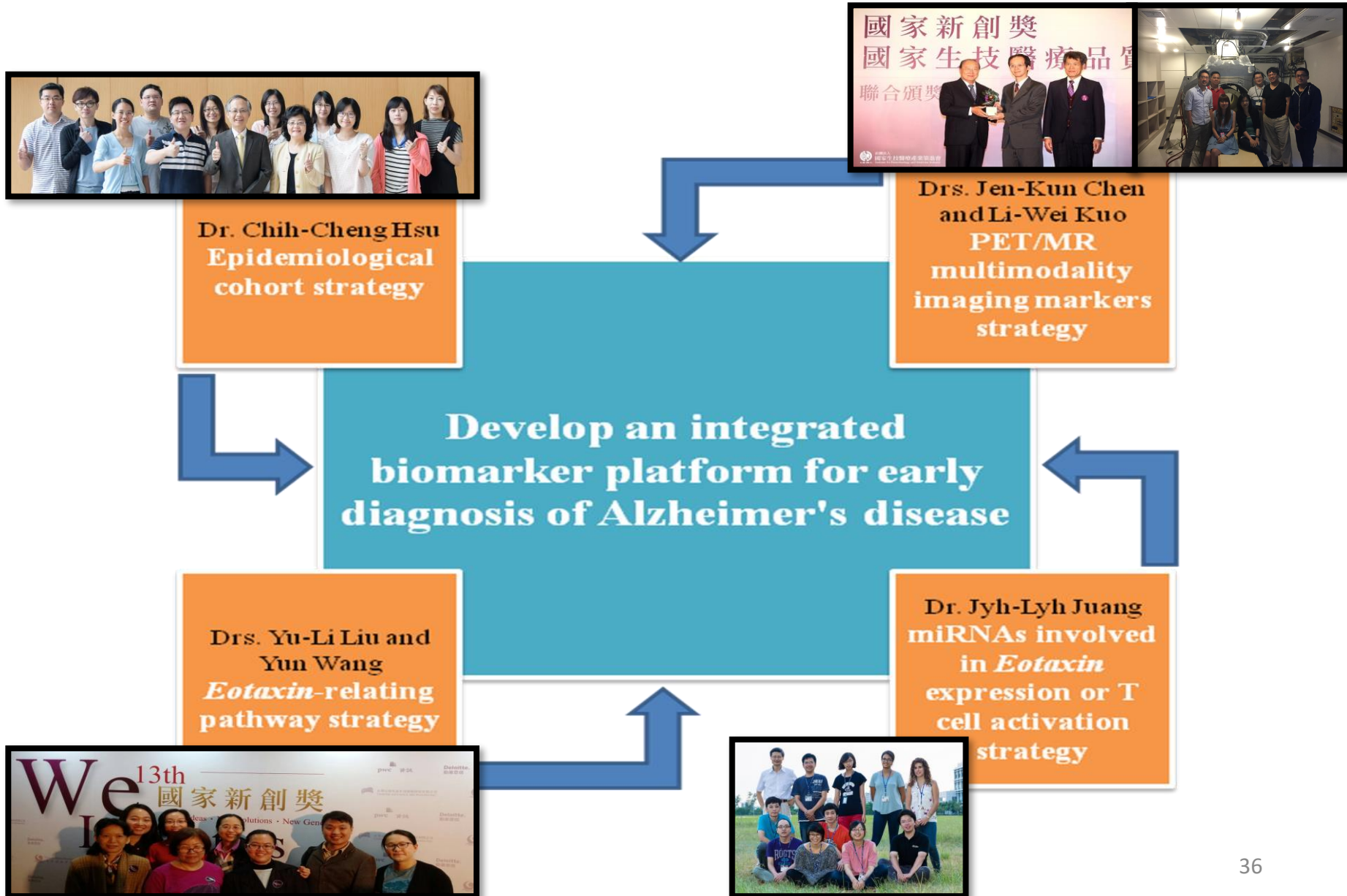
bilateral supplementary/pre-supplementary motor and right ventral premotor areas

# **Application Example: Brain Network Analysis using Graph Theory on Dementia**

# Preface

- Patients suffering from Alzheimer's disease (AD) are often diagnosed after progressively altered behavior, which are difficult to distinguish from the symptoms of mild cognitive impairment (MCI).
- **Neuroimaging approaches** provides anatomical, functional and metabolic information non-invasively and have been considered as promising tools to improve the diagnosis of AD.
- Brain network analysis utilizing graph theory could be potentially helpful to distinguish AD from MCI or even early aging. A joint development with machine learning approach for classification is also emergently needed.

# Dementia research team at NHRI



# Materials and Methods

## ➤ Patient recruitment

- All the clinical assessments and experiments were performed in Dalin Tzu-Chi Hospital. A total of **71** subjects were recruited in MR study, including **26** healthy control subjects (HC), **22** MCI and **23** AD.

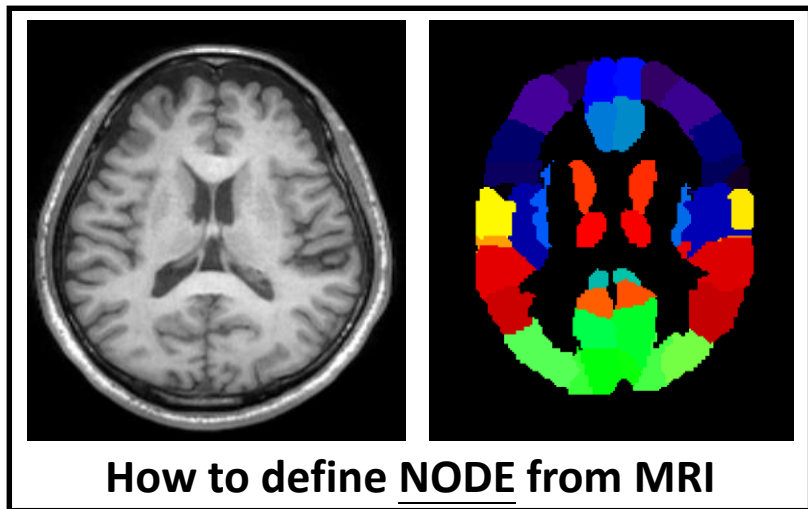
## ➤ MR experiments

- All MR experiments were performed on a 1.5T MRI scanner (HDxt, GE, USA). For brain functional network, we acquired 3D T1-weighted images and resting-state functional MRI data. For structural network, we acquired DTI data with 30 gradient directions ( $b = 1000 \text{ s/mm}^2$ ).

## ➤ Analysis approaches

- In this study, we incorporated both statistical and machine-learning approaches on brain network measures to investigate the functional alterations of brain in AD and aimed to establish a useful framework for classifying HC, MCI and AD.

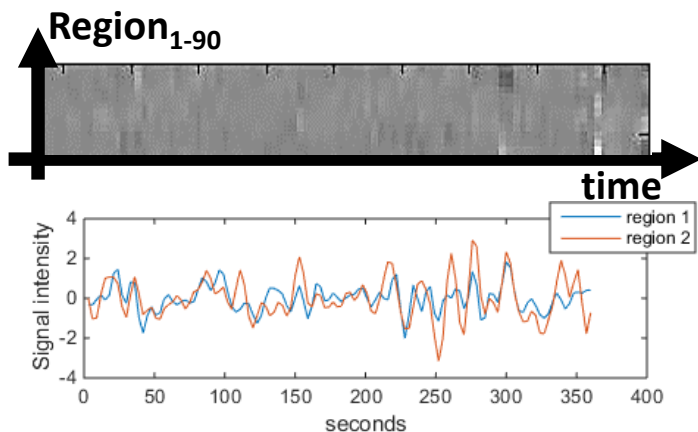
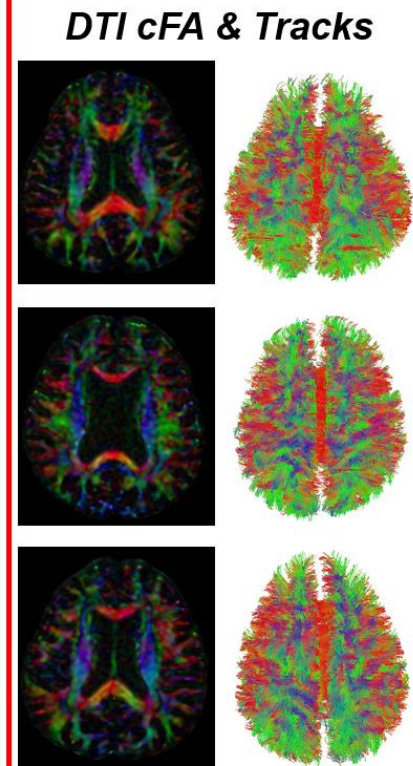
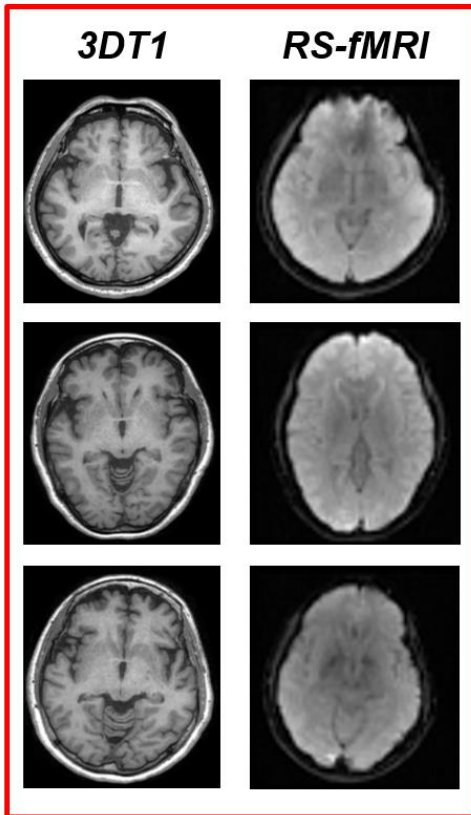
# Brain Functional Network Analysis



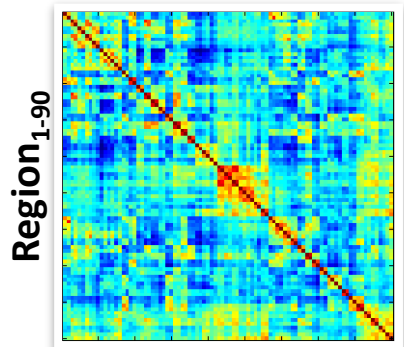
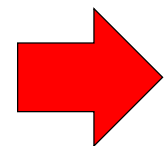
Healthy

MCI

AD



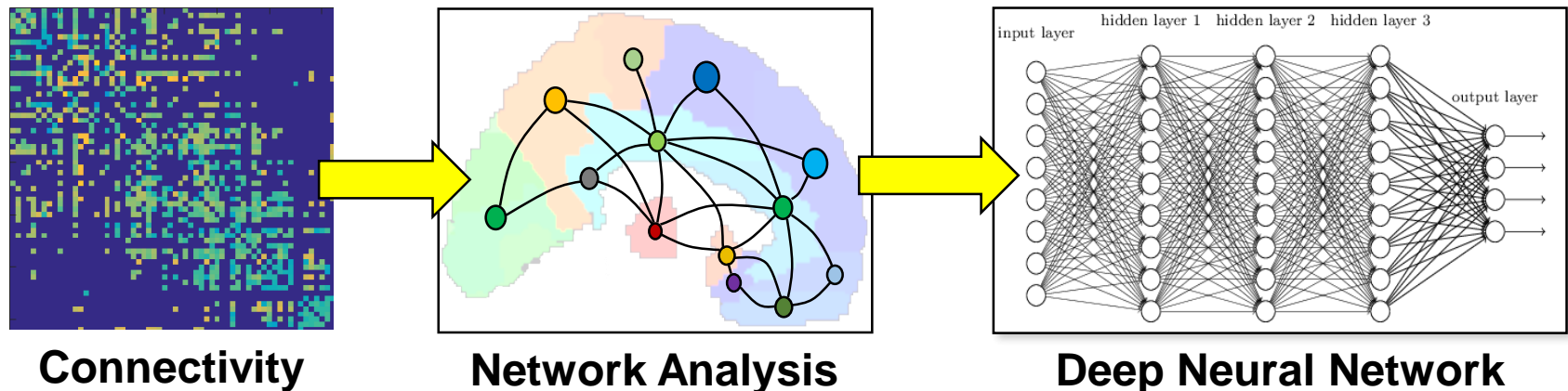
*Functional connectivity calculation*



*Functional network matrix*

# Build a deep neural network model

- In this work, we aimed to establish a classification model based on brain network analysis and deep neural network
- The classification accuracies using different types of functional connectivity were compared



# Comparison of functional connectivity on classification accuracy

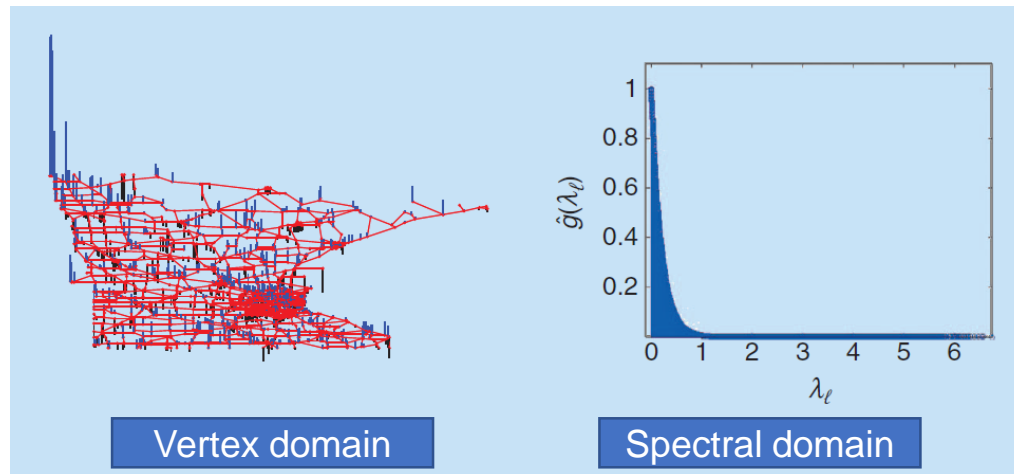
- Normalized fMRI time series (across 90 AAL regions) was used for functional connectivity calculation
  - **Pearson's correlation, covariance, normalized mutual information (NMI) and GSP graph learning**
- Connectivity matrix sparsification
  - **For Pearson's, covariance and NMI, the sparsification range is [0.1 0.3]**
  - **For GSP, no sparsification is needed**
- Four kinds of network measures were used as features in training model
  - **Nodal degree, clustering coefficient, local efficiency, pagerank centrality**



# Graph Signal Representations in Spectral Domains

- The Graph Fourier Transform can be defined on the vertices of a graph and represent graph signals on spectral domain

$$\hat{f}(\lambda_\ell) := \langle f, \mathbf{u}_\ell \rangle = \sum_{i=1}^N f(i) u_\ell^*(i). \quad f(i) = \sum_{\ell=0}^{N-1} \hat{f}(\lambda_\ell) u_\ell(i).$$

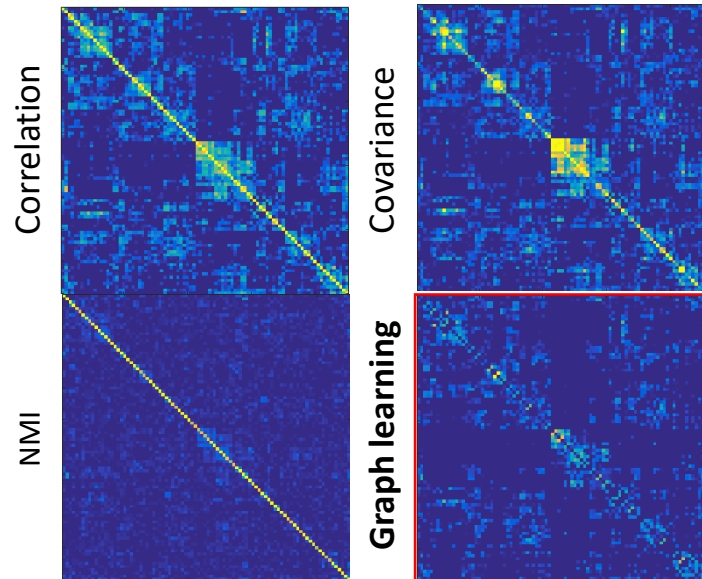


*A graph on vertex domain and its corresponding spectrum domain (Shuman et al., 2013)*

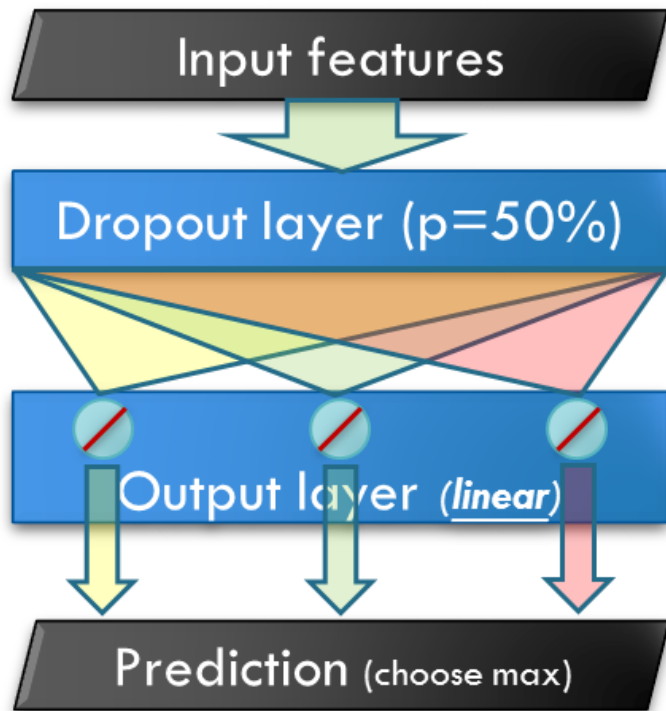
# Graph Signal Processing

- **Relationship between eigenvectors and frequency**
  - Eigenvectors associated with small eigenvalues indicate the signals vary slowly across the graph
  - Eigenvectors associated with large eigenvalues indicate the signals oscillate rapidly and are more likely to have dissimilar values on adjacent vertices

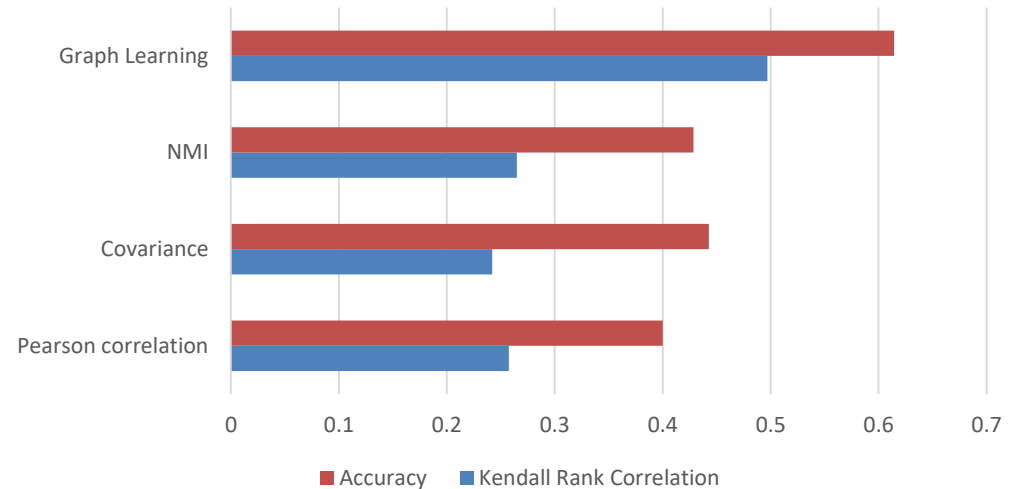
***In our work, we utilize graph learning technique (Kalofolias et al., AISTATS 2016) to process the functional connectivity matrix by maximizing smoothness of signals on the graph***



# Classification of HC/MCI/AD using deep neural network



**Architecture of the Classifier  
Implemented using TensorFlow**

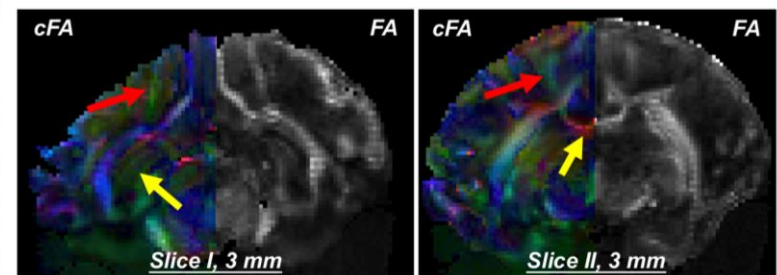
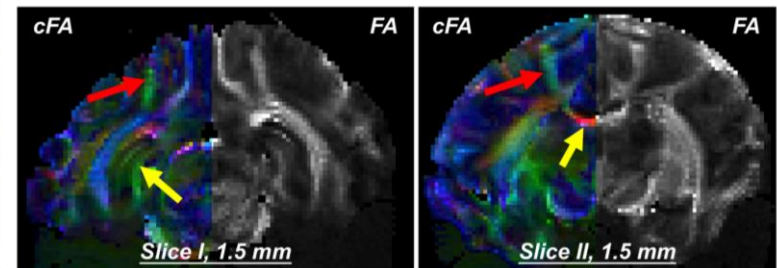
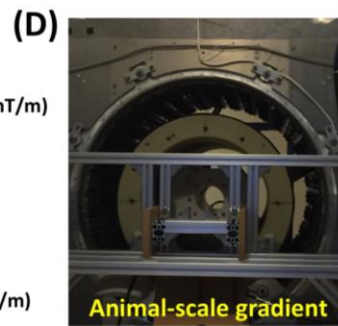
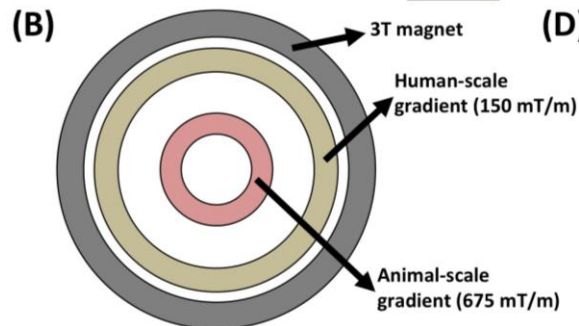
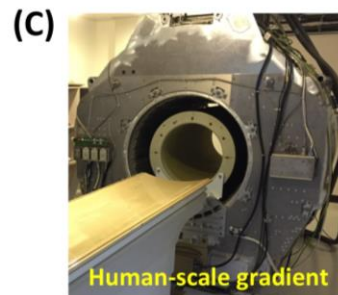
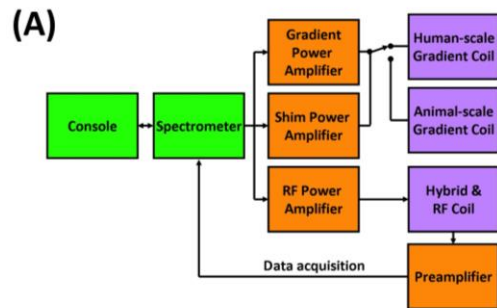
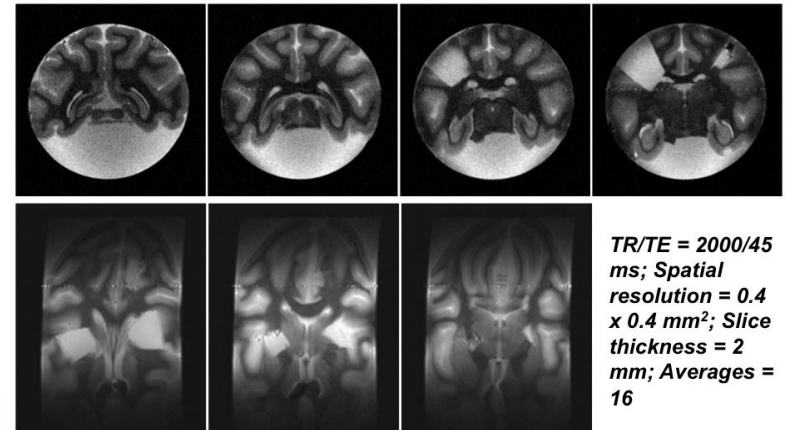
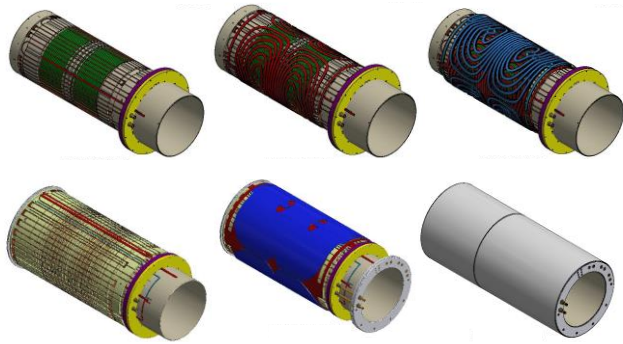


Connectivity	Pearson corr.	Covariance	NMI	Graph learning
Accuracy	0.4	0.44	0.43	0.61

# Summary

- The AI has significantly changed the development of medical imaging instrumentations during the past few years. More coming in future!
  - ✓ *Although potentially useful, its reliability and validity on clinical use still needs further investigation*
- Graph theoretical analysis could be potentially useful in identifying altered network topologies of brain structures and functions
  - ✓ *A joint development with deep learning is highly expected*
- **”Data” is the “key”**: to enhance the data quality by building a *high-performance dedicated brain MRI*

# A high-performance dedicated brain 3T MRI at NHRI



# ***Acknowledgements***



**We greatly thank for the financial supports from  
NHRI, MOST, MOHW and MOEA**